## **Cotransport-Induced Instability of Membrane Voltage in Tip-Growing Cells**

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A salient feature of stationary patterns in tip-growing cells is the key role played by the symports and antiports, membrane proteins that translocate two ionic species at the same time. It is shown that these cotransporters destabilize generically the membrane voltage if the two translocated ions diffuse differently and carry a charge of opposite (same) sign for symports (antiports). The orders of magnitude obtained for the time and length scale are in agreement with experiments. A weakly nonlinear analysis characterizes the bifurcation.

DOI: [10.1103/PhysRevLett.95.208105](http://dx.doi.org/10.1103/PhysRevLett.95.208105) PACS numbers: 87.10.+e, 05.65.+b, 87.16.Uv

Spatiotemporal pattern formation of the electric membrane potential in cells and tissues emerges from collective dynamics and activity of membrane ion channels. Action potential and cardiac excitation spiral waves are paradigmatic examples of nonstationary pattern formation [1,2]. Stationary patterns of ionic currents are widespread in fungi, plant cells (algae, for example), protozoa, and insects: Chara corallina, Fucus zygote, and Achlya are the model cells [3,4]. Such patterns are correlated to cell polarization, apical growth, morphogenesis, and nutrient acquisition. The characteristic wavelengths and times vary from a few millimeters to 10  $\mu$ m and from 1 h to 1 min, respectively. These times correspond typically to a membrane protein or an ion diffusive time. Two mechanisms have been proposed [5]: one based on the electromigration of membrane proteins [6–10] and the other resulting from a negative differential conductance characterizing voltagegated channels [11–13].

However, the origin of current patterns is still unclear in tip-growing cells where transcellular currents are mainly produced by the pump and a cotransporter, a membrane carrier that translocates two species of ions at the same time [14,15] (see Fig. 1). Three points of view are proposed by biologists for tip-growing cells: ionic currents may be a consequence of cellular growth, a self-organized pattern coupled to growth, or, alternatively, arise as a selforganized pattern which precedes cellular growth [16]. The appearance of a lateral branching preceded by an inward current supports the hypothesis of self-organization in Achlya [15]. The mechanisms proposed in the literature cannot explain such patterns [17].

In this Letter, we ask the broader question: How does the stability of the membrane voltage depend on cotransporters? Only the contribution of channels to membrane voltage instability has been investigated in the literature. We demonstrate here that the voltage along a membrane containing cotransporters is linearly unstable on a diffusive (not electrical) characteristic time. The final pattern is a stationary modulation of ionic concentrations, membrane voltage, and transcellular ionic currents. The mechanism is specific to this kind of carrier since each ionic transporter is characterized by a *positive* differential conductance.

Consider two ions 1, 2 of valence numbers  $z_i$  and concentrations *Cj*, diffusing along a cylindrical cellular membrane of radius *r*. As in the cable model, the electrodynamics is governed by a one-dimensional electrodiffusive equation for each ion,

$$
\partial_t C_j = D_j \partial_x^2 C_j + z_j (e D_j / k_B T) \partial_x (C_j \partial_x V) - (2/r) J_j, \quad (1)
$$

and the capacitive relation for the membrane voltage *V*,

$$
V = V_0 + (Fr/2C_m)[z_1(C_1 - C_{10}) + z_2(C_2 - C_{20})], \quad (2)
$$

where  $D_j$  is the diffusion coefficient of ion *j*,  $V_0$  the resting membrane potential ( $\approx$  - 0.1 V),  $C_m$  the specific membrane capacitance ( $\approx 0.01 \text{ F m}^{-2}$ ), and  $C_{j0}$  the concentration of ion *j* in the resting state. The standard cable model is recovered simply from (1) and (2) when all ionic diffu-



FIG. 1. The pump (not drawn) generates a gradient of the electrochemical potential through the membrane by translocating continuously one species of ions (gray disk). This stored free energy is used by the symport, a cotransporter, to transfer a second species of ion (black disk) or nutrient against its own gradient if necessary. The stoicheiometry of the drawn symport is equal to 2: two gray disks for one black disk.

sion coefficients are identical. In our model, the fluxes  $J_i$ take into account the intracellular chemical reactions as well as the membrane fluxes through pumps, cotransporters, channels, and uniports. The pump uses chemical energy [adenosine triphosphate (ATP)] to translocate ions from one side to the other (the 1-ion in this Letter), generating an electrochemical potential gradient through the membrane: for example, H<sup>+</sup>-ATPase in plant cells. Consequently, the 1-ion is a cation. Cotransporters use this stored free molar energy to transfer one 2-ion for *n* 1-ions in the same (opposite) sense for the symport (antiport) carrier (see Fig. 1). In practice, the stoicheiometry *n* is equal to either 1 or 2. In tip-growing cells, the 2-ion is often an essential nutrient for future vegetal metabolism and consequently, implied in many chemical processes based on enzymatic binding reactions, metabolism in Achlya hyphae with the methionine (an amino acid) uptake or the carbon dioxide supply to chloroplasts for photosynthesis in Chara corallina by  $HCO_3^-$  entry. Finally, the flux  $J_i$  of each ion *j* is

$$
J_1 = J_{\text{pch}} + nJ_s,\tag{3}
$$

$$
J_2 = \pm J_s + \alpha C_2 + J_2^{\text{NL}}, \tag{4}
$$

where  $J_{\text{pch}}$  is the flux through active pumps and passive channels translocating the 1-ion,  $\pm J_s$  ( $nJ_s$ ) is the flux of the 2-ion (1-ion) through the cotransporter, and  $J_2^{\text{NL}}$  is the (concentration-dependent) nonlinear part of  $J_2$ , due to intracellular chemical processes. The mechanism of the (linear) voltage instability does not depend on the functional form of  $J_2^{\text{NL}}$ . The characteristic kinetic constant  $\alpha$ of nutrient uptake is necessarily positive. The sign  $\pm$  is  $+$ for a symport and  $-$  for an antiport. In the following, we consider the case of the symport but the extension to that of the antiport is straightforward. For simplicity's sake,  $J_{\text{peh}}$  and  $J_s$  do not depend on concentrations and vary linearly with the membrane potential *V*, characterized by their positive conductances:  $G_{\text{pch}} = z_1 F(\partial J_{\text{pch}}/\partial V)$  and  $G_s = z_1 F(\partial J_s/\partial V)$ . Even if a cotransporter is often called a secondary active carrier, its working is passive. Consequently, the differential conductance of the current through the cotransporter,  $(n + z_2/z_1)G_s$  is always positive (positive Onsager coefficient). Then, there is no local positive feedback provided by protein characteristics. In the homogeneous resting state,  $J_j = 0$  for each ion: the molar flux  $J_{s0}$  of the nutrient uptake in the resting state may be nonzero. Equations  $(1)$ – $(4)$  are scaled with dimensionless coordinates for space  $x' = x/\lambda$  and time  $t' = t/\tau$ with the cable length characteristic of the pumps and channels (primes are then dropped for simplicity),  $\lambda^2 = r\gamma/2G_{\text{pch}}$ , and the diffusive time  $\tau = \tilde{D}\lambda^2/D_1D_2$ , where  $\gamma$  is the bulk ionic conductivity and  $\tilde{D} = \delta_1 D_1 +$  $\delta_2 D_2$  is the mean coefficient of diffusion. We set  $\delta_j =$  $z_j^2 C_{j0}/(z_1^2 C_{10} + z_2^2 C_{20})$  equal to 0.5 in all the following.

The control parameter  $\mu$  is the positive conductance ratio,  $\mu = G_s/G_{\text{pch}}$ , that controls the ionic membrane fluxes. The stability of the homogeneous equilibrium state is analyzed by considering the evolution of fluctuations of voltage *V* and ionic concentrations  $C_i$  and consequently the linearized equations of (1)–(4):  $\delta H(x, t) = \delta H_0 e^{st + ikx}$ , where *k* is the wave number of the perturbation and *H* refers to *V* and  $C_j$ . Two real solutions for  $s = s(k)$  are determined: Im(s) = 0, Re(s) =  $\sigma(\mu; k)$ . The first one is the well-known fast capacitive relaxation. The second one yields the growth rate of the instability:

$$
\sigma(\mu; k) = -\frac{k^4 + \frac{\tilde{D}}{D_1}k^2[1 + \mu(n + \frac{D_1 z_2}{D_2 z_1})]}{k^2 + 1 + (n + z_2/z_1)\mu} - \frac{\beta_1}{D_2}
$$

$$
\times \frac{(\tilde{D} - D_2)k^2 + (D_1 - D_2)(1 + n\mu)\frac{\tilde{D}}{D_1}}{k^2 + 1 + (n + z_2/z_1)\mu}, \quad (5)
$$

where  $\beta_1 = \alpha \gamma / G_{\text{pch}}(D_1 - D_2)$  is dimensionless. Since the capacitance does not appear in (5), this characteristic (inverse) time is *diffusive*. From  $\sigma(\mu_0(k); k) = 0$ , the neutral curve  $\mu_0(k)$  is determined and has a minimum defining the critical values of the control parameter  $\mu_c$  and the wave number  $k_c$  (Fig. 2):

$$
\mu_c = \frac{-D_1 D_2}{\tilde{D}(z_2 D_1/z_1 + nD_2)} \left[ 2k_c^2 + \frac{\tilde{D}}{D_1} + \beta_1 \left( \frac{\tilde{D}}{D_2} - 1 \right) \right],
$$
  

$$
(k_c^2 - k_0^2)^2 = k_0^4 + \frac{\beta_1 \tilde{D}}{D_1 D_2} (D_1 - D_2)
$$

$$
+ k_0^2 \left[ \frac{\tilde{D}}{D_1} + \beta_1 \left( \frac{\tilde{D}}{D_2} - 1 \right) \right],
$$

where  $k_0^2 = -n\beta_1(D_1 - D_2)/(z_2D_1/z_1 + nD_2)$ . The particular case  $\alpha = \beta_1 = 0$  corresponds to a long-wavelength instability  $(k_c = 0)$ , and will not be treated here [9].



FIG. 2. The neutral curve  $\mu_0(k)$  is defined by  $\sigma(\mu_0(k); k) = 0$ and has a minimum at  $(k_c; \mu_c)$ . Above the critical control parameter  $\mu_c$ , the membrane voltage is unstable. Parameters are  $n = 2$ ,  $z_1 = 1$ ,  $z_2 = -1$ ,  $D_1 = 10^{-5}$  cm<sup>2</sup> s<sup>-1</sup>,  $D_2 =$  $10^{-7}$  cm<sup>2</sup> s<sup>-1</sup> (common for the three neutral curves), and  $\beta_1$  = 0.1 (solid line),  $\beta_1 = 0.2$  (dashed line), and  $\beta_1 = 0.3$  (dotted line).

For  $\mu > \mu_c > 0$ , the growth rate is positive in a finite range of wave numbers. The limit case of small binding reactions may help clarify the nature of this instability. For small but nonzero  $\beta_1$ , the homogeneous resting state is unstable  $(\sigma > 0)$  against spatial perturbations if 1 +  $\mu(n + D_1 z_2/D_2 z_1)$  < 0. Recalling that  $0 \le n + z_2/z_1$ , two necessary conditions for instability are  $D_1$  >  $nD_2|z_1/z_2|$  and  $z_2/z_1 < 0$  [18]. The former is generally verified since binding reactions reduce notably the effective diffusion of the 2-ion [19]; the latter is fulfilled for the symports  $H^+/HCO_3^-$  in Chara corallina and H--methionine in Achlya. For large control parameter  $\mu$  and small  $\beta_1$ , the wavelength  $\lambda_p$  of the pattern satisfies:  $\lambda_p \approx 2\pi (r \gamma D_2 / 2G_s \tilde{D})^{1/2} \approx \lambda_{\text{cable}} (D_2 / \tilde{D})^{1/2}$ , where  $\lambda_{\text{cable}}$  is provided by the cable model and may be experimentally measured by two impaled electrodes. An order of magnitude of  $\lambda_p$  can thus be evaluated. In Achlya hyphae, some measurements indicate  $\lambda_{\text{cable}} \approx 2 \text{ mm}$  [20]. On the basis of measurements of the effective diffusion of the calcium ion, a reasonable value for the diffusion coefficient of the 2-ion is  $D_2 \approx 10^{-7}$  cm<sup>2</sup>/s. We thus expect a characteristic pattern wavelength  $\lambda_p \approx 100 \ \mu \text{m}$ , in agreement with experiments. The characteristic time  $\tau_p$  required to produce the pattern is of the order of a diffusive time:  $\tau_p \approx$  $\lambda_p^2/D_2$ , dominated by the slower ionic diffusion. Using the previous values, we find  $\tau_p \approx 10^3$  s, in agreement with experiments on Achlya hyphae [3].

Equations  $(1)$ – $(4)$  have been solved numerically for a large range of parameters to confirm the previous results. For simplicity, the nonlinear flux  $J_2^{\text{NL}}$  is given by a truncated expansion in powers of the concentration of the 2 ion:

$$
J_2^{\text{NL}} = C_{20} \sum_{j=2,3} \alpha_j [(C_2 - C_{20})/C_{20}]^j.
$$
 (6)

This form generalizes the expansion of a Michaelis-Menten enzyme kinetics term in the limit of large Michaelis constant: our goal is to take into account at a phenomenological level some of the complexity due to the function of the 2-ion. The coefficient  $\alpha_3$  must be positive to ensure nonlinear convergence. The simulation depends on two additional dimensionless parameters:  $\beta_2 = \gamma^2 |V_0| \alpha_2 / [z_2 F G_{\text{pch}} C_{20} (D_1 - D_2)^2]$  and  $\beta_3 =$  $\gamma^{3}|V_{0}|^{2}\alpha_{3}/[(z_{2}F)^{2}G_{\text{pch}}C_{20}^{2}(D_{1}-D_{2})^{3}]$ . Generally, the voltage relaxes to zero on a characteristic capacitive time, as expected from the cable model. However, for relevant parameters characterizing a symport, a cellular pattern of voltage and concentrations appears after a transient whose duration is of the order of magnitude of the diffusive time  $\tau_p$  (Fig. 3). Outer and inner transcellular currents flow periodically through the membrane. It has been established that the Ohmic part  $I_{Ohm}$ of the dimensionless extracellular current normal to the membrane is given by the following relation:  $I_{Ohm}$  =



FIG. 3. Parameters are the same as in Fig. 2, with additional  $\mu = 0.25, \beta_1 = 0.1, \beta_2 = 0.1, \text{ and } \beta_3 = 5.$  (a) The final stationary pattern is a modulation of the dimensionless membrane potential  $(V - V_0)/|V_0|$  (solid line) and of the dimensionless Ohmic part  $I_{Ohm}$  (dashed line) of the extracellular current. An hyperpolarized membrane potential  $(V - V_0)/|V_0| < 0$  corresponds to an outer Ohmic current (electric field) in agreement with experiments made with the vibrating probe. (b) Temporal evolution of the extracellular current *I*<sub>Ohm</sub> at the position  $x = 12.5$ . The characteristic time is an ionic diffusive one.

 $\tilde{D}(I_1/D_1 + I_2/D_2)/G_{\text{pch}}|V_0|$  [12]. An outer (inner) ohmic current corresponds to an hyperpolarized (depolarized) band in agreement with experiments (Fig. 3). The outer current has a characteristic M shape, observed in Chara corallina. Varying the nonlinear parameters, it is possible to obtain a M shape only for the inner current or for both.

The stationary bifurcation is further characterized by a weakly nonlinear analysis performed in the vicinity of the threshold  $(k_c; \mu_c)$  [2]. An arbitrarily small expansion parameter  $\epsilon$  is introduced to separate the fast and slow scales in the problem. We define the slow independent variables  $X = \epsilon x$  and  $T = \epsilon^2 t$ , and Taylor expand the concentrations  $C_i$ , membrane voltage *V*, and control parameter  $\mu$  in powers of  $\epsilon$ . The resulting equations are then solved recursively for each power  $\epsilon^i$ . The solvability condition (Fredholm alternative) at third order provides the amplitude equation:

$$
\tau_0 \partial_T A = \bar{\mu} A + \xi_0^2 \partial_X^2 A - g|A|^2 A, \tag{7}
$$

where  $\bar{\mu} = (\mu - \mu_c)/\mu_c$  is the reduced control parameter. The time and length scale  $\tau_0$  and  $\xi_0$  of the pattern's slow modulations close to the bifurcation may also be derived directly from the dispersion relation (5):  $\mu_c \xi_0^2 = \frac{1}{2} (\partial \xi_0^2 - \partial \eta_0^2)$  and  $\tau^{-1} = \mu_c (\partial \xi_0^2 - \eta_0^2)$ . The coeffi- $\frac{1}{2}(\partial^2 \mu_0 / \partial k^2)_c$  and  $\tau_0^{-1} = \mu_c(\partial \sigma / \partial \mu)_c$  [2]. The coefficient *g* of the nonlinear term is a complicated function of the physical parameters. The bifurcation is supercritical (subcritical) for positive (negative) values of *g*. In the



FIG. 4. The tricritical line  $g = 0$  separates domains in the reduced parameter space  $(D_2/D_1; \beta_3)$  where the bifurcation is supercritical  $(g > 0)$  and subcritical  $(g < 0)$ . The fixed parameter values are the same as in Fig. 3.

idealized case described here, and for typical parameter values, a tricritical line  $g = 0$  separates the two types of bifurcation in parameter space (see Fig. 4).

In conclusion, we established that a spatially homogeneous membrane voltage is linearly unstable if the cotransporters play a role in the control of the electrophysiological properties of a cell. The final stationary pattern is a transcellular current bearing various ionic species. As opposed to many other scenarios leading to spatiotemporal pattern formation in ionic currents [1,11,12], a negative differential conductance is not required. A necessary ingredient is the slow intracellular diffusion of one of the two ions translocated by the cotransporter. Interestingly, this is often the case in experiments. This mechanism may explain how a cell can uptake an essential nutrient at precise locations: in Achlya, methionine enters at the tip during apical growth.

We thank P. Pelcé for useful discussions. We wish to acknowledge the support of ''ACI Physico-chimie des systèmes complexes" (France), the Fonds National de la Recherche Scientifique (Belgium), and the Communauté Française de Belgique-Action de Recherches Concertées (Belgium).

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