

Responses of a Hodgkin-Huxley neuron to various types of spike-train inputs

Hideo Hasegawa

Department of Physics, Tokyo Gakugei University, Koganei, Tokyo 184, Japan

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Numerical investigations have been made of responses of a Hodgkin-Huxley (HH) neuron to spike-train inputs whose interspike interval (ISI) is modulated by deterministic, semi-deterministic (chaotic), and stochastic signals. As deterministic one, we adopt inputs with the time-independent ISI and with time-dependent ISI modulated by sinusoidal signal. The Rössler and Lorentz models are adopted for chaotic modulations of ISI. Stochastic ISI inputs with the gamma distribution are employed. It is shown that distribution of output ISI data depends not only on the mean of ISIs of spike-train inputs but also on their fluctuations. The distinction of responses to the three kinds of inputs can be made by return maps of input and output ISIs, but not by their histograms. The relation between the variations of input and output ISIs is shown to be different from that of the integrate and fire (IF) model because of the refractory period in the HH neuron.

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I. INTRODUCTION

Neurons in our brain are known to be responsible for encoding the characteristics of stimuli into a form for further processing by other neurons. During the last decades, anatomical, physiological, and theoretical studies on neurons have been extensively made. Despite these efforts, the code used for encoding and decoding in neurons has not been clarified at the moment [1]. It is commonly believed that the firing rate reflects the strength of the inputs which trigger the action potentials of neurons. Indeed, the firing activities of motor and sensory neurons vary in response to the applied stimuli. It is not known, however, whether the information is carried through the mean firing rate (rate encoding) or through the details of sequences of the temporarily encoded interspike interval (ISI) (temporal encoding), which is currently controversial [2–4]. In the last few years, experimental evidences have accumulated, indicating that many biological systems use the temporal coding. Human visual systems, for example, have shown to classify patterns within 150 msec in spite of the fact that at least ten synaptic stages are involved from retina to the temporal brain [5]. The similar speed of visual processing has been reported for macaque monkeys [6]. Because the firing frequency of neurons involved is less than 100 Hz, each neuron can contribute at most one or two spikes to such computations; there is not sufficient time to sample firing rates.

In recent years, many studies on the encoding of the spike trains by neurons have been made by using the integrate and fire (IF) model [7], which is one of the simplest, dynamical models of neurons [8]. The IF neuron is silent without the external, input current I_i . When I_i exceeds the critical value I_{ic} , the IF neuron shows the self-excited oscillations, whose frequency f_o depends on the magnitudes of I_i . It is shown that f_o continuously vanishes when I_i is decreased and approaches to I_{ic} . This behavior of the continuous $f_o - I_i$ dependence is different from the discontinuous one at I_{ic} in the more realistic Hodgkin-Huxley (HH) neurons [9]; the IF and HH neurons are classified as the type I and type II, respectively [10]. Furthermore, the IF neuron has the disadvantages of the artificial reset of the action potential and the

lack of the refractory period. Although it has been widely employed for the study of neural networks, the IF model is too crude to discuss the activities of real neurons.

The HH model, which well describes the spiking behavior and refractory properties of real neurons, is expressed based on non-linear conductances of Na and K ion channels [9]. Since the HH model was proposed, its property has been intensively investigated [11–17]. The behavior of self-excited oscillations of the HH neuron with the applied current has much variety than that of the IF model. It is shown that the oscillation of the HH neuron may become chaotic when the sinusoidal I_i is applied with proper choices of magnitude and frequency [16,17]. Such chaotic oscillations are experimentally observed in squid giant axons [14,15] and Onchidium neurons [18].

The HH model was originally proposed to account for the property of squid giant axons [9] and it has been generalized with modifications of ion conductances [19]. The HH-type models have been widely adopted for a study on activities of *transducer neurons* such as motor and thalamus relay neurons, which transform the amplitude-modulated input to spike-train outputs. In this paper, we pay our attention to *data-processing neurons* which receive and emit the spike-train pulses. Assuming that the data-processing neuron may be essentially described by the ion-conductance mechanism of the HH model, we investigate its input-output response in order to get some insight into the following questions.

(1) How the output ISIs depend on the input ISIs? Does the average rate of the output ISI depend only on the average of the input ISIs?

(2) How do neurons distinguish the different types of deterministic, chaotic, and stochastic inputs? How different is the response to different types of spike-train inputs?

Our paper is organized as follows. In the next Sec. II, we mention a simple neuron model adopted for our numerical calculation. In Sec. III, we investigate the response of our system to deterministic inputs with time-independent ISI (Sec. III A) and time-dependent ISIs modulated by sinusoidal signal (Sec. III B). Input and output ISIs are studied by their histograms and return maps; the former shows the distributions and the latter the time correlation of ISI data. In Sec.

IV, chaotic inputs generated by Rössler (Sec. IV A) and Lorenz model (Sec. IV B) are discussed. Stochastic inputs with the gamma distribution are treated in Sec. V. The final Sec. VI is devoted to conclusion and discussion.

II. ADOPTED MODEL

We adopt a simple system consisting of a neuron and a synapse. The neuron is assumed to be described by the HH model and the synapse by the alpha function [Eq. (16)]. We will investigate the response of our neuron when spike-train inputs are applied through the synapse.

The HH model is described by the nonlinear coupled differential equations for the four variables, V for the membrane potential and m , h , and n for the gating variables of Na and K channels, and it is given by [9]

$$CdV/dt = -g_{\text{Na}}m^3h(V - V_{\text{Na}}) - g_{\text{K}}n^4(V - V_{\text{K}}) - g_{\text{L}}(V - V_{\text{L}}) + I_i, \quad (1)$$

$$dm/dt = -(a_m + b_m)m + a_m, \quad (2)$$

$$dh/dt = -(a_h + b_h)h + a_h, \quad (3)$$

$$dn/dt = -(a_n + b_n)n + a_n, \quad (4)$$

where

$$a_m = 0.1(V + 40)/[1 - e^{-(V+40)/10}], \quad (5)$$

$$b_m = 4e^{-(V+65)/18}, \quad (6)$$

$$a_h = 0.07e^{-(V+65)/20}, \quad (7)$$

$$b_h = 1/[1 + e^{-(V+35)/10}], \quad (8)$$

$$a_n = 0.01(V + 55)/[1 - e^{-(V+55)/10}], \quad (9)$$

$$b_n = 0.125e^{-(V+65)/80}. \quad (10)$$

Here the reversal potentials of Na, K channels and leakage are $V_{\text{Na}} = 50$ mV, $V_{\text{K}} = -77$ mV, and $V_{\text{L}} = -54.5$ mV; the maximum values of corresponding conductivities are $g_{\text{Na}} = 120$ mS/cm², $g_{\text{K}} = 36$ mS/cm², and $g_{\text{L}} = 0.3$ mS/cm²; the capacity of the membrane is $C = 1$ μ F/cm². Details of the HH model can be found in Refs. [9,20].

The external, input current, I_i , is taken to consist of two terms:

$$I_i = I_s + I_p \quad (11)$$

where I_s expresses the static dc current and I_p denotes the pulse current induced by the spike-train input whose explicit form will be discussed shortly [Eq. (15)].

We consider the delta-function-type spike-train input expressed by

$$U_i(t) = V_a \sum_n \delta(t - t_{in}). \quad (12)$$

The firing time t_{in} for arbitrary n is assumed to be recurrently defined by

$$t_{in+1} = t_{in} + T_{in}, \quad (13)$$

$$t_{i1} = 0, \quad (14)$$

where the ISI of input spike T_{in} is generally a function of a given time t_{in} . In this study, we take T_{in} to be constant ISI, and time-dependent ISI modulated by sinusoidal, chaotic, and stochastic signals.

The spike train given by Eq. (12) is assumed to be injected through the synapse, yielding the current I_p given by

$$I_p(t) = g_{\text{syn}} \sum_n \alpha(t - t_{in})(V_a - V_{\text{syn}}). \quad (15)$$

Here g_{syn} and V_{syn} are the conductivity and reversal potential of synapse, and the alpha function $\alpha(t)$ is defined by [20]

$$\alpha(t) = (t/\tau)e^{-t/\tau}\Theta(t), \quad (16)$$

where τ is the time constant relevant to the synapse conduction and $\Theta(t)$ is the Heaviside step function. When the ISI is very large compared with τ , Eqs. (15) and (16) yield pulse currents with the maximum value of $I_p^{\text{max}} = e^{-1}g_{\text{syn}}(V_a - V_{\text{syn}})$ at $t = t_{in} + \tau$ and with the half-width of 2.45τ . We assume $V_a = 30$ mV (the typical value of the maximum membrane potential), $V_{\text{syn}} = -50$ mV and $\tau = 2$ msec, and treat g_{syn} as a parameter.

When the membrane potential V oscillates, it yields the spike-train output, which may be expressed by

$$U_o(t) = V_a \sum_m \delta(t - t_{om}), \quad (17)$$

in a way similar to Eq. (12), and the output ISI is given by

$$T_{om} = t_{om+1} - t_{om}. \quad (18)$$

We will investigate how T_{om} depends on the various types of T_{in} .

Differential equations given by Eqs. (1)–(10) including the external current given by Eqs. (11)–(16) are solved by the forth-order Runge-Kutta method for 20 sec with the integration time step of 0.01 msec. We discard results of initial ten thousand steps to get asymptotic solutions. If ISI of spike-train input or output is about 10 msec, the size of its sample is about 2000. Although this figure is not sufficiently large for statistics of ISI data, we hope an essential ingredient will be clarified in our numerical investigation.

III. DETERMINISTIC INPUTS

A. Time-independent ISI

1. Pacemaker neurons

Let us first consider the HH neuron without the spike-train input ($I_p = 0$). The HH neuron is reported to be silent for $I_s = 0$, and to show the self-excited oscillation when I_s exceeds the critical value of $I_{ic} = 6.3$ μ A/cm², above which T_{on} decreases gradually as I_s is increased. The dashed curve in Fig. 1(d) expresses an example of the self-excited oscillation with the period of $T_{on} = 10.75$ msec for $I_s = 25$ μ A/cm² and $I_p = 0$.

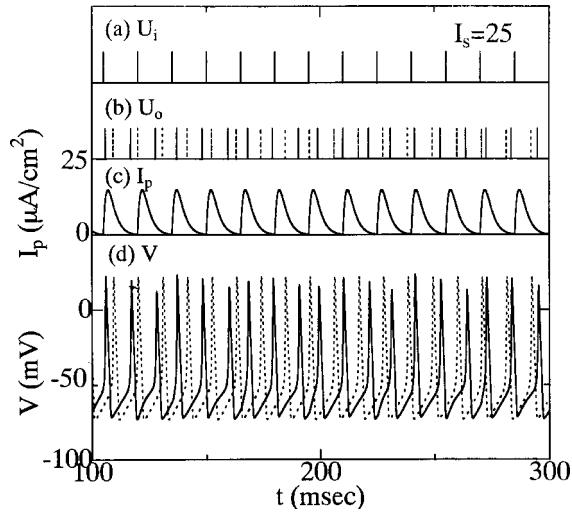


FIG. 1. Responses of the self-excited HH neuron to the time-independent input ISI [I_p with $T_i = 15$ msec and $I_s = 25$ $\mu\text{A}/\text{cm}^2$]; time sequences of (a) input U_i , (b) output U_o , (c) pulse current I_p , and (d) membrane potential V . Dashed curves in (b) and (d) the result with $I_p = 0$.

Now we apply the spike-train input to this self-excited neuron. The input is given by Eqs. (10)–(16) with the time-independent ISI of $T_{in}(t_{in}) = T_i = 15$ msec and $g_{syn} = 0.5$ mS/cm². This spike-train input U_i shown in Fig. 1(a) yields the pulse current I_p shown in Fig. 1(c), by which the membrane potential V oscillates as depicted by the solid curve in Fig. 1(d). We plot in Fig. 1(b) the time sequence of the spike-train output U_o which should be compared with the input U_i . The pulse current I_p has the maximum value of $I_p^{\max} = 14.8$ $\mu\text{A}/\text{cm}^2$ at $t = t_{in} + \tau$ msec. We notice that the oscillation in V is rather different from that shown by the dashed curve for $I_p = 0$. Figure 2 expresses the histogram of the output ISI, showing that $\{T_o\}$ distributes continuously between 8.36 to 11.62 msec. The mean and root-mean-square (rms) values of the output ISI are $\mu_o = 10.43$ and $\sigma_o = 1.12$ msec, respectively. This oscillation is chaotic as was pointed out for the HH neuron receiving sinusoidal inputs [16,17]; the pulse current I_p shown in Fig. 1(c) is not so different from the sinusoidal one in a crude sense. The chaotic behavior is clearly seen in Fig. 3, which depicts return maps of input and output ISIs.

When the ISI value of spike-train input $T_i (= \mu_i)$ is changed, we get an interesting behavior in μ_o as shown in

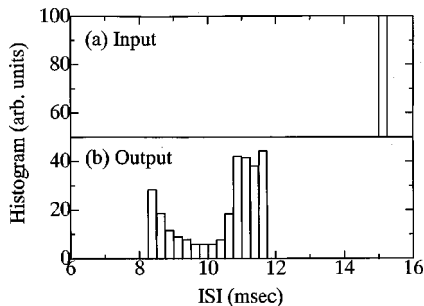


FIG. 2. Histograms of (a) the time-independent input ISI ($T_i = 15$ msec) and (b) output ISI of the self-excited neuron (see Fig. 1).

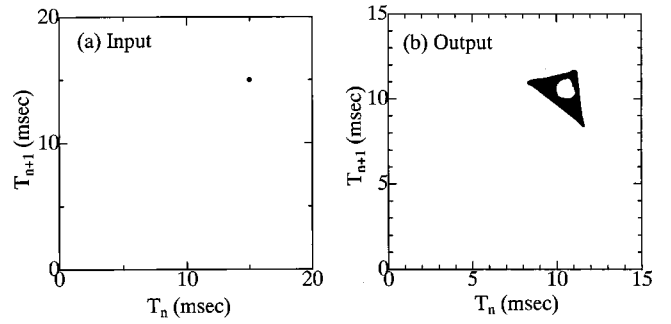


FIG. 3. Return maps of (a) time-independent input ISI with $T_i = 15$ msec and (b) output ISI of the self-excited neuron (Fig. 1).

Fig. 4, where the solid (dashed) curve expresses μ_o (σ_o), and filled circles express the distribution of $\{T_{on}\}$ for a given μ_i . We note that for $\mu_i = 9 - 11$ msec, the period of the oscillation is forced to be the same; $T_{om} = T_i$, leading to the ratio $k \equiv \mu_o / \mu_i = 1$. When $\mu_i = 5$ msec, we get $\mu_o = 10$ msec and then $k = 2$. On the contrary, for $\mu_i = 20$ msec, we get the two values of $T_{on} = 9$ and 11 msec, and $\mu_o = 10$, the average period of the output being a half of the input ($k = 1/2$). This is also the case for $\mu_i = 21$ and 22 msec. In the other cases noticed above, the ISI of output distributes between about 8.5–11.5 msec. We should note that irrespective of μ_i , output ISI is always about 10 msec, which is nearly equal to $T_o = 10.75$ msec, ISI for $I_s = 25$, and $I_p = 0$ $\mu\text{A}/\text{cm}^2$.

2. Silent neurons

Next consider the silent neuron with $I_s = 0$, for which the oscillation of the membrane potential is induced by applied spike-train inputs. Figures 5(a)–5(d) show the calculated result in which the spike-train input is given by $T_{in} = \mu_i = 10$ msec and $g_{syn} = 0.5$ mS/cm² without static currents ($I_s = 0$). The applied spike-train inputs shown in Fig. 5(a) create the pulse current with the peaks of $I_p^{\max} = 15.3$ $\mu\text{A}/\text{cm}^2$ as shown in Fig. 5(c). The induced oscillation of the membrane potential V in Fig. 5(d) is phase locked with the ratio of 4:3, oscillating with a long cycle of 40.00 msec ($= 11.25 + 12.36 + 16.39$) = 4 μ_i , where 11.25, 12.36, and 16.39 are the values of output ISIs. The return map of output ISIs is plotted in Fig. 6(a).

Figure 7 shows μ_o and σ_o as a function of μ_i . We notice that μ_o agrees with μ_i ($k = 1$) for μ_i greater than 12 msec,

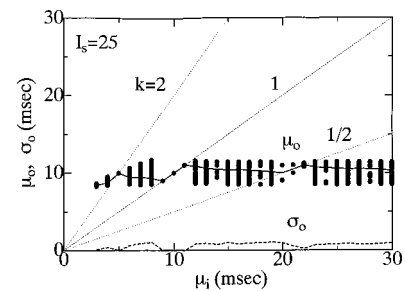


FIG. 4. Mean (μ_o , solid curve) and rms (σ_o , dashed curve) values of output ISI of self-excited neurons ($I_s = 25$ $\mu\text{A}/\text{cm}^2$) against the mean value (μ_i) of time-independent input ISI. Filled circles denote the distribution of output ISIs for a given μ_i , dotted curves denoting $k \equiv \mu_o / \mu_i$.

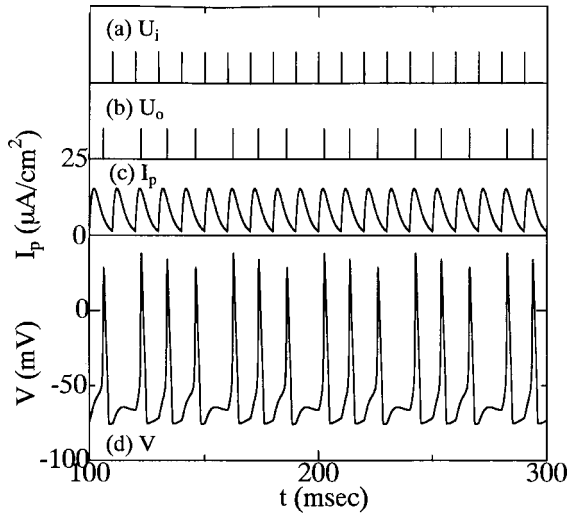


FIG. 5. Response of the silent HH neuron to the time-independent input ISI (I_p with $T_i=10$ msec and $I_s=0$); time sequences of (a) the input U_i , (b) output U_o , (c) pulse current I_p , and (d) membrane potential V .

where the HH neuron behaves as a simple transmitter with a delay of about 2.0 msec. This is in strong contrast with the behavior of the self-excited neuron discussed in the preceding subsection (Fig. 4). On the other hand, for μ_i less than 11 msec, the behavior of output ISI is rather complicated. It is easy to see that $k=2$ for $\mu_i=6, 7,$ and 8 msec, and that $k=3$ for $\mu_i=4$ msec. For $\mu_i=9$, we get $T_{om}=12.06$ and 14.96 msec, leading to a longer period of $3\mu_i=27.00$ ($= 12.06 + 14.96$) msec. For $\mu_i=5$ msec, we get $T_{om}=10.94$ and 14.06 msec, which leads to a long period of $5\mu_i=25$ msec, its return map being shown in Fig. 6(b). Surprisingly, a much longer period of $13\mu_i$ is realized for $\mu_i=11$ msec. The rms value of σ_o has an appreciable value only around $\mu_i=10$ msec.

We have repeated our calculation by changing the value of g_{syn} . The calculated ratio, $k=\mu_o/\mu_i$, is shown as functions of g_{syn} and μ_i in Fig. 8, where only the integer values of k are shown. Note that noninteger values of k exist between the integer values; for example, $k=4/3$ for $g_{syn}=0.5$ mS/cm² and $\mu_i=10$ msec (Fig. 7). We cannot obtain spike-train outputs for small synaptic couplings as expected. When $\mu_i=10$ msec, we get the critical value of $g_{syn}=0.11$ mS/cm² below which no outputs are available. This coupling yields the pulse current with the maximum value of

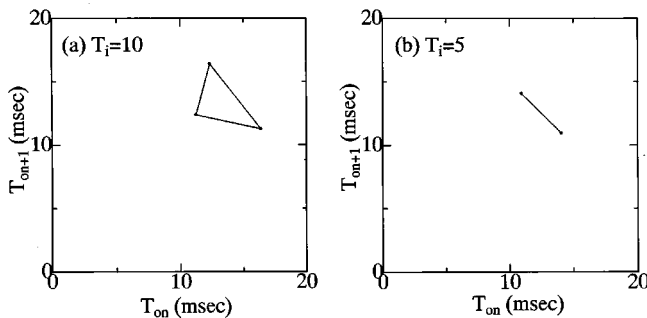


FIG. 6. Return maps of output ISIs for the time-independent input with (a) $T_i=10$ and (b) 5 msec (see Fig. 5).

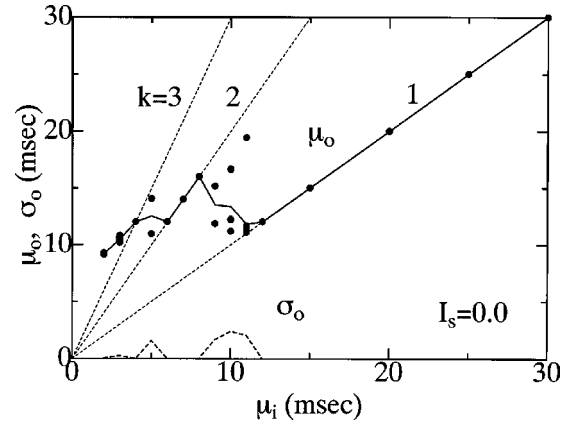


FIG. 7. Mean (μ_o , solid curve) and rms (σ_o , dashed curve) values of output ISI of silent neurons against the mean value (μ_i) of time-independent input ISI. Filled circles denote the distribution of output ISIs for a given μ_i , dotted curves denoting $k\equiv\mu_o/\mu_i$.

$I_p^{max}=1.6$ $\mu\text{A}/\text{cm}^2$, which is much smaller than the critical dc current of $I_{ic}=6.3$ $\mu\text{A}/\text{cm}^2$ for the self-excited oscillation with $I_p=0$. We note that we get $k=1$ for the large ISIs with fairly strong synaptic couplings. When we decrease μ_i with keeping g_{syn} fixed, values of k become larger since the HH neuron cannot respond to inputs with the small ISI because of its refractory period. Figure 8 reminds us the result of Guttman, Feldman, and Jakobson [15] who reported in their Table 1, the calculated k as functions of the magnitude A and the frequency f_i when the sinusoidal input given by $I_i=A\sin(2\pi f_i t)+I_b$ is applied to squid giant axons with a bias current I_b . Our result for $\mu_i<10$ msec agrees fairly with that of Ref. [15]. However, the agreement between the two results is not good for $\mu_i\geq 10$ msec, where our input current with the pulse width of about $2.45\tau\sim 5$ msec [Eqs. (15) and (16)] is quite different from the sinusoidal current adopted in Ref. [15].

As was shown in Fig. 4, the self-excited HH neuron emits the output ISI of $T_{om}\sim 10$ msec irrespective of the value of input ISI, and then it is considered to be inadequate as a data processor. Then, in the following sections, we will investigate only the silent HH neuron with a fixed value of $g_{syn}=0.5$ mS/cm².

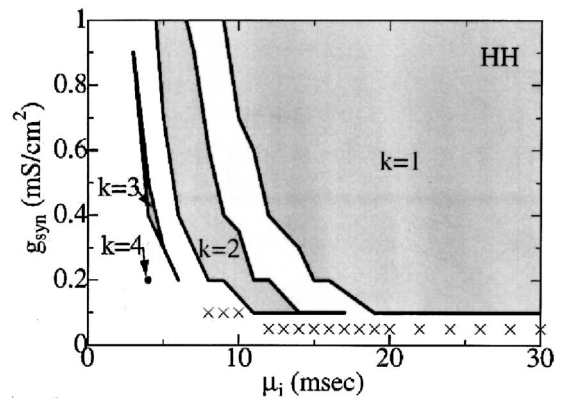


FIG. 8. The phase diagram of the calculated ratio of k ($=\mu_o/\mu_i$) in the μ_i-g_{syn} space for the time-independent ISI input to silent neurons: only integer k 's are shown and crosses denote no outputs (see text).

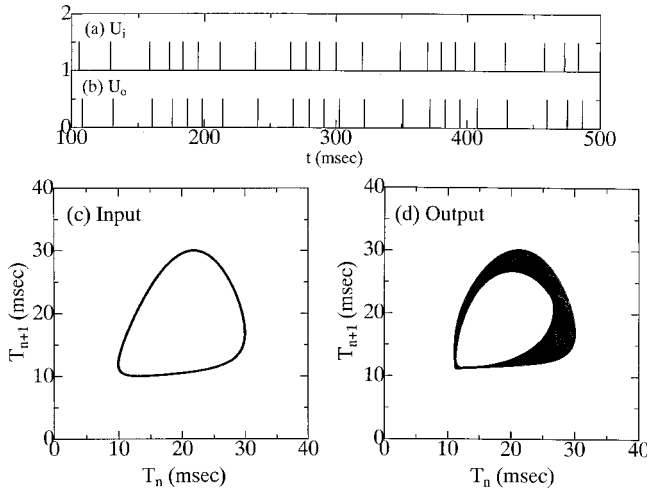


FIG. 9. Time courses of (a) input U_i and (b) output U_o , and return maps of (c) input and (d) output ISIs for the sinusoidal modulation for $d_0=2d_1=20$ msec [Eq. (19)].

B. ISI with sinusoidal modulation

In this subsection we discuss an application of the spike-train input whose ISI is modulated by the sinusoidal signal given by

$$T_{in}(t) = d_0 + d_1 \sin(2\pi t/T_p), \quad (19)$$

where T_p is the period and d_0 and d_1 are coefficients adjusting μ_i and σ_i .

Figures 9(a) and 9(b) show the time course of input U_i and output U_o for $d_0=2d_1=20$ msec with $T_p=100$ msec. Because of the introduced sinusoidal modulation, ISIs at $100 < t < 150$ msec are, for example, larger than those at $150 < t < 200$ msec. Figure 9(c) depicts the return map of input ISIs, which has the egg-shape circle expected for the sinusoidal signal. On the other hand, the return map of output ISIs shown in Fig. 9(d) reveals the chaotic behavior. Results for $d_0=2d_1=10$ are plotted in Figs. 10(a)–10(d), which show that although the return map of input ISI has the egg-shape circle, that of output ISIs is distorted. The reason

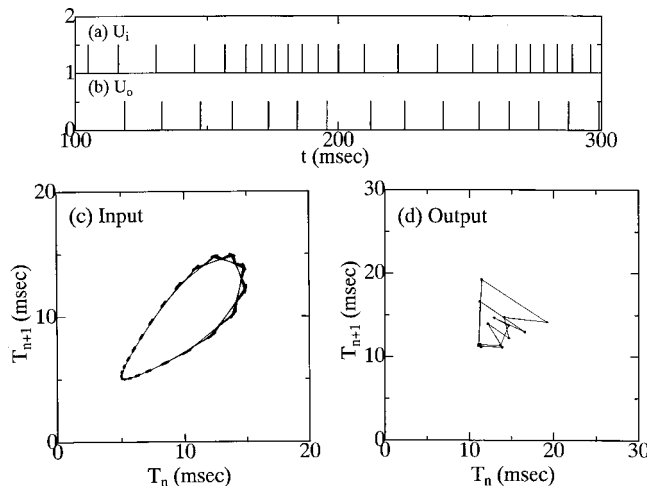


FIG. 10. Time courses of (a) input U_i and (b) output U_o , and return maps of (c) input and (d) output ISIs for the sinusoidal modulation for $d_0=2d_1=10$ msec [Eq. (19)].

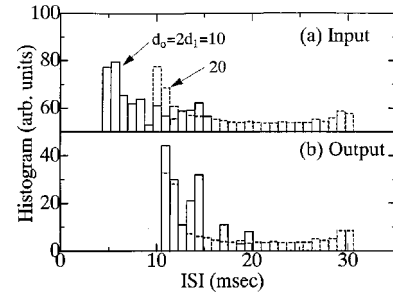


FIG. 11. Histograms of (a) input ISI with sinusoidal modulation and (b) output ISI. Solid (dashed) curves are for $d_0=2d_1=10$ (20) msec.

of this distortion is explained in Fig. 11, where solid histograms express input and output ISIs for $d_0=2d_1=10$ ($\mu = 8.68$, $\sigma = 3.42$) and dashed histograms those for $d_0=2d_1=20$ ($\mu_i = 17.54$, $\sigma_i = 6.94$), with $T_p=100$ msec. (It is noted that we get $\mu_i < d_0$ because the histogram of the input ISI at $T_{in} < d_0$ has larger magnitudes than that at $T_{in} > d_0$.) In the case of $d_0=2d_1=20$ msec, the input and output ISIs distribute almost in the same region at $11 < T_{om} < 30$ msec. On the contrary, in the case of $d_0=2d_1=10$ msec, the output ISIs distribute at $11.01 < T_{om} < 19.48$ msec while input ISIs are at $5.00 < T_{in} < 14.96$ msec; no output ISIs at $T_{om} < 11$ msec. This is due to the refractory period of the HH neuron and it is the origin of the distortion in the return map shown in Fig. 10(b). Defining the dimensionless coefficients of variations for input and output ISIs by

$$c_{v\lambda} = \sigma_\lambda / \mu_\lambda, \quad (\lambda = i \text{ and } o) \quad (20)$$

we get $c_{vo} = 0.17$ and 0.38 for $d_0=2d_1=10$ and 20 msec, respectively; note that $c_{vi} = 0.40$ for both inputs.

Figure 12 shows μ_o and σ_o calculated by changing μ_i with the fixed value of $c_{vi} = 0.40$. Solid and dashed curves denote μ_o and σ_o , respectively, and filled circles the distribution of $\{T_{om}\}$ for a given μ_i . We notice that there is no output ISIs with T_{om} less than about 10 msec, which shows characteristic of the low-pass filter of the silent HH neuron.

IV. CHAOTIC INPUTS

A. Rössler model

In this section, we study the spike-train input whose ISI is modulated by chaotic signals. First we adopt the Rössler model, which is given by

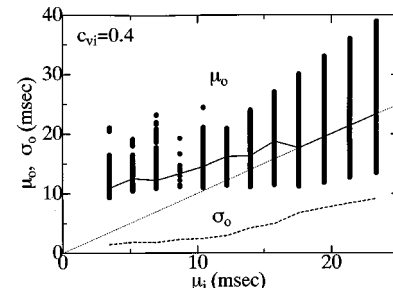


FIG. 12. Mean (μ_o , solid curve) and rms (σ_o , dashed curve) values of output ISI against the mean value (μ_i) of input ISI with sinusoidal modulation ($c_{vi} = 0.40$). Filled circles denote the distribution of output ISIs for a given μ_i , dotted curves denote $k \equiv \mu_o / \mu_i = 1.0$.

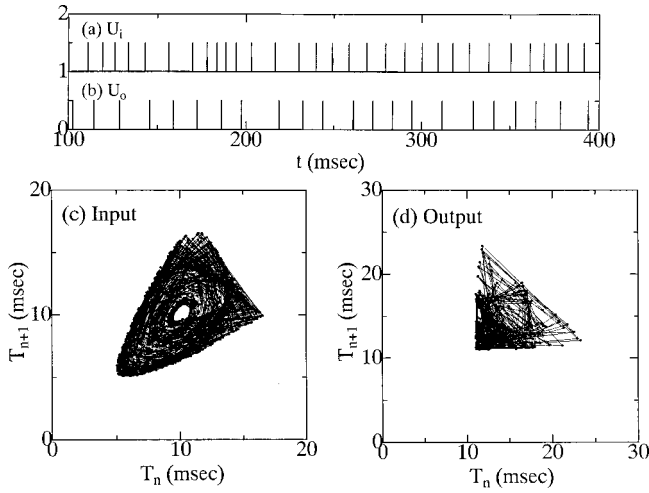


FIG. 13. Time courses of (a) input U_i and (b) output U_o , and return maps of (c) input and (d) output ISIs for chaotic inputs generated by the Rössler model (case R1).

$$dx/dt = -y - z, \quad (21)$$

$$dy/dt = x + ay, \quad (22)$$

$$dz/dt = bx - cz + xz, \quad (23)$$

with $a=0.36$, $b=0.4$, and $c=4.5$ [21]. Since ISI has to be positive and the characteristic time scale in the Rössler model is different from that of the HH model, we adopt the variable $x(t)$ which yields

$$T_{in}(t_{in}) = d_0 + (d_1/10)x(pt_{in}), \quad (24)$$

with the following two choices of parameters:

$$d_0 = d_1 = 10 \text{ msec and } p = 1/10 \text{ (case R1),}$$

$$d_0 = d_1 = 20 \text{ msec and } p = 1/20 \text{ (case R2).}$$

Figures 13(a) and 13(b) show the time course of input and output spike trains for the case R1. The return map of input ISI depicted in Fig. 13(c) shows a shape characteristic for chaotic signals. On the other hand, the return map of output ISIs is rather strange with no traces at $T_o < 10$ msec. This is due to the low-pass filter behavior of the silent HH neuron,

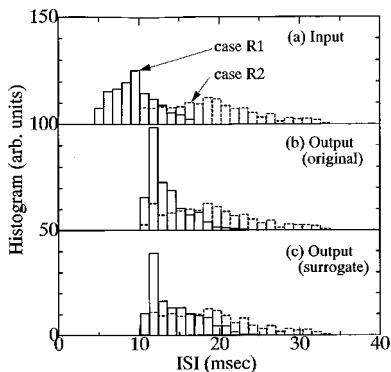


FIG. 14. Histograms of (a) input ISI and (b) output ISI for the chaotic input generated by the Rössler model, and (c) output ISI for its surrogate, solid (dashed) curves being for case R1 (R2).

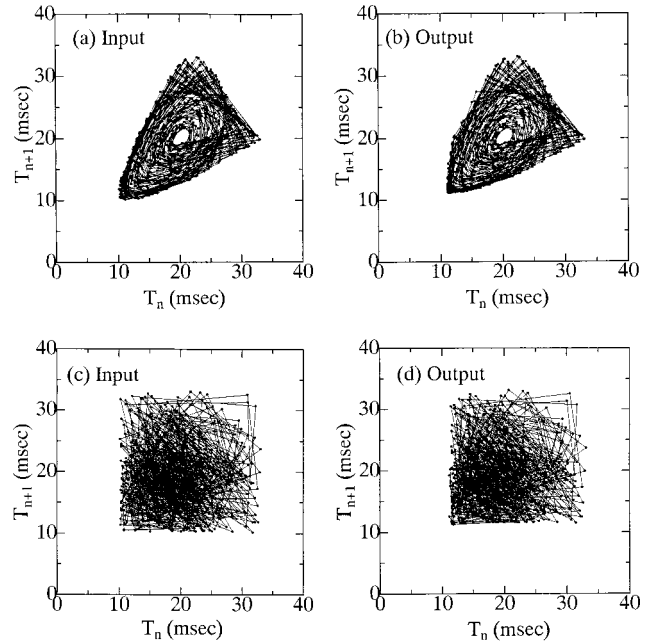


FIG. 15. Return maps of (a) input ISI and (b) output ISI for the chaotic input generated by the Rössler model (case R2); (c) and (d) are corresponding return maps of its surrogate data.

as shown by solid histograms in Figs. 14(a) and 14(b); output ISIs distribute at $11.11 < T_{om} < 25.15$ msec ($\mu_{om} = 13.43$, $\sigma_o = 2.44$ msec) whereas input ISIs distribute at $5.06 < T_{in} < 16.56$ msec ($\mu_i = 9.53$, $\sigma_i = 2.69$ msec).

Return maps for the case R2 are shown in Fig. 15, in which both return maps are almost the same. This is because input and output ISIs locate almost in the same region of $10 < T_{in}, T_{om} < 30$ msec, as shown by dashed histograms in Figs. 14(a) and 14(b).

Next we investigate the nature of the correlation in the ISI sequences. This is made by employing the surrogate data method applied to ISI data [23]. We adopt the shuffled surrogate as a simple method to get surrogate data. The distributions of ISIs of shuffled surrogate inputs are exactly the same as those of original ISI data although surrogate data have no time correlation between successive ISI values.

The time course of the membrane potentials for the surrogate data is ostensibly quite similar to that for the original chaotic input (not shown). The solid (dashed) histogram in Fig. 14(c) shows the distribution of output ISIs of surrogate data generated from the Rössler model for the case R1 (R2). The results of the surrogate data are similar to those for the corresponding original data. Return maps of the input and output ISI of the surrogate data, depicted in Figs. 15(c) and 15(d), show the characteristics of random signals.

B. Lorentz model

The similar calculation is made with the use of the Lorentz model, which is given by

$$dx/dt = d(y - x), \quad (25)$$

$$dy/dt = ex - y - xz, \quad (26)$$

$$dz/dt = -fz + xy, \quad (27)$$

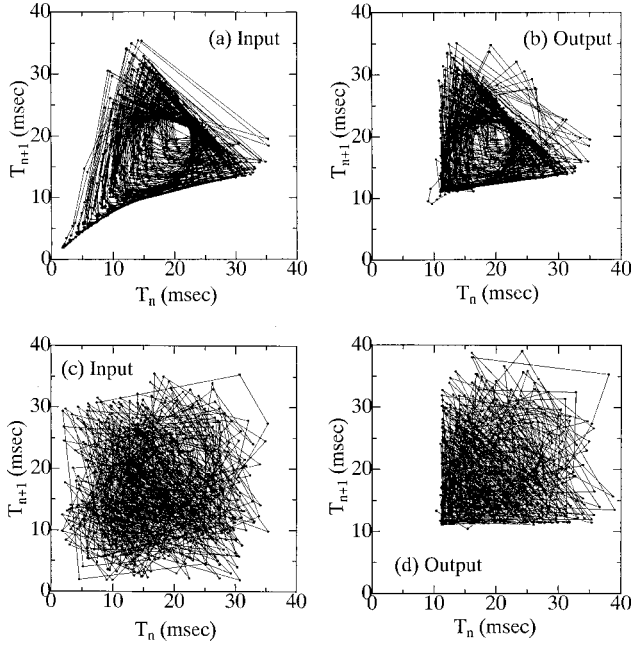


FIG. 16. Return maps of (a) input ISI and (b) output ISI for the chaotic input generated by the Lorentz model; (c) and (d) are corresponding return maps of its surrogate data.

with $d = 10$, $e = 28$, and $f = 8/3$ [22]. We employ the variable $z(t)$, with which the input ISI is given by

$$T_{in}(t_n) = d_0 + (d_1/25) [z(pt_{in}) - 25], \quad (28)$$

where $d_0 = d_1 = 20$ and $p = 1/100$.

Figures 16(a)–16(d) show return maps of ISI data of original chaotic data and its surrogate. Return maps of output ISIs for the chaotic and surrogate data shown in Figs. 16(b) and 16(d) have no traces at $T_{om} > 10$ msec because of the low-pass filter character of the HH neuron.

Sauer [24], and Racicot and Longtin [25] studied the response of the IF model to the input whose amplitudes are modulated by chaotic signals. It was shown that when the mean firing rate is high, the relationship between input and output is high, which leads to the high nonlinear predicability. Our calculations, on the other hand, have shown that when the mean firing rate is too high (i.e., input ISIs are too short such as $T_{in} < 10$ msec), the information is lost because the HH neuron behaves as the low-pass filter due to its refractory period, which is not included in the IF model.

V. STOCHASTIC INPUTS

The ISIs of spike-train input T_{in} in Eq. (13) are assumed to be independent random variables with the gamma probability density function given by

$$P(T) = s^r T^{r-1} e^{-sT} / \Gamma(r) \quad (29)$$

for which we get $\mu_i = r/s$, $\sigma_i = \sqrt{r/s}$, and $c_{vi} = 1/\sqrt{r}$, $\Gamma(r)$ being the gamma function. It is noted that in the limit of $r = 1$, Eq. (29) reduces to the exponential distribution ($c_{vi} = 1$) and that in the limits of $r \rightarrow \infty$ and $s \rightarrow \infty$ with keeping $\mu_i = r/s$ fixed, Eq. (29) reduces to $P(T) = \delta(T - \mu_i)$, the constant ISI with $\mu_i = T$ and $c_{vi} = 0$.

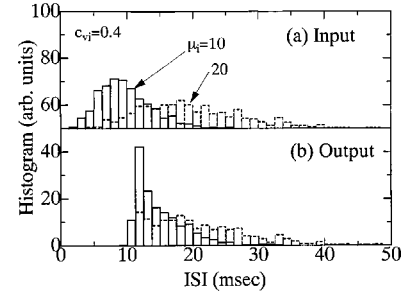


FIG. 17. Histograms of (a) input ISI and (b) output ISI for spike-train inputs with the gamma distribution; solid (dashed) curves for input ISIs of $\mu_i = 10(20)$ msec with $c_{vi} = 0.40$.

The spike-train input created by the gamma-distribution generator is applied to our neural system. Calculations are performed by changing μ_i by keeping the value of c_{vi} fixed. Note that because the size of our sample of input ISI is not sufficiently large, the obtained c_{vi} fluctuates around the intended values. Solid histograms in Figs. 17(a) and 17(b) show the result for $c_{vi} = 0.40$, $\mu_i = 10$ msec, $c_{vo} = 0.25$, and $\mu_o = 14.84$ msec while dashed histograms for the result for $c_{vi} = 0.40$, $\mu_i = 20$ msec, $c_{vo} = 0.36$, and $\mu_o = 21.11$ msec.

Solid and dashed curves in Fig. 18(a) denote μ_o and σ_o , respectively, for $c_{vi} = 0.4$. We note that as increasing μ_i , μ_o increases and approaches the dotted line expressing $\mu_o = \mu_i$. This is similar to the case of $c_{vi} = 0$ shown in Fig. 7, where $\mu_o = \mu_i$ at $\mu_i \geq 10$ msec. On the contrary, the dependence of μ_o on μ_i for the case of $c_{vi} = 1.0$ shown in Fig. 18(b), is rather different from the cases of $c_{vi} = 0$ and 0.4. We get $\mu_o \sim (\mu_i + 10)$ msec at $\mu_o < 100$ msec and it deviates from the dotted line showing $\mu_o = \mu_i$. These calculations depicted in Figs. 18(a) and 18(b) clearly show that μ_o de-

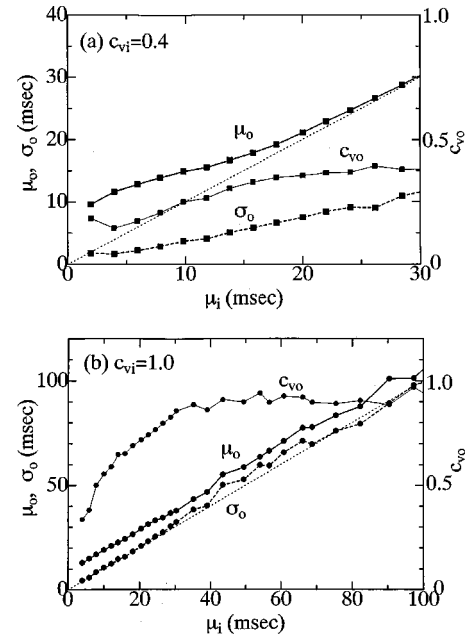


FIG. 18. Mean (μ_o , solid curves), rms (σ_o , dashed curves), and c_{vo} (thin solid curves) of output ISIs against the mean value (μ_i) of input ISI for gamma distribution with (a) $c_{vi} = 0.4$ and (b) $c_{vi} = 1.0$. The dotted curves denoting $\mu_o = \mu_i$ are plotted as guides for the eye.

pends not only on μ_i but also on σ_i (c_{vi}). Although both μ_o and σ_o increase as the value of μ_i is increased, the increase in the latter is more significant than that in the former, which yields an increase in c_{vo} , as shown by the thin-solid curves in Figs. 18(a) and 18(b). We note that c_{vo} approaches the values of c_{vi} as increasing μ_i , the related discussion being given in Sec. VI.

We have performed the calculation also using input ISI with random, uniform distribution. Obtained results are similar to those for the gamma distribution, as far as the adopted values of c_{vi} are the same (not shown).

VI. CONCLUSION AND DISCUSSION

We have investigated the responses of the HH neurons, by applying the various types of spike-train inputs whose ISI is modulated by deterministic, chaotic, and stochastic signals. The obtained results are summarized as follows.

(1) Output ISIs of the self-excited HH neuron against the time-independent input ISI are always $T_{om} \sim 10$ msec irrespective of the value of the input ISI (Fig. 4).

(2) Output ISIs of the silent HH neurons for the constant ISI with $T_{in} > 10$ msec yield output ISI with $T_{om} = T_{in}$ whereas for ISI with $T_{in} < 10$ msec, the HH neuron generally emits multiple kinds of output ISIs (Fig. 7).

(3) For the input ISI modulated by sinusoidal, chaotic, and stochastic signals, the silent HH neuron behaves as a low-pass filter because of its refractory period, yielding output ISI with $T_{om} > 10$ msec.

(4) Output ISIs generally depend not only on the mean of the input ISI but also on their fluctuations: the HH neuron is not a simple integrator.

(5) The analysis on the histograms of input and output ISIs cannot distinguish the responses to the deterministic, chaotic, and stochastic signals.

(6) The distinction can be made by an analysis of the time correlation of the ISI data, for example, by plotting their return maps.

Softky and Koch [26] have reported a large coefficient of variability ($c_{vo} = 0.5 \sim 1.0$) for spike trains of non-bursting cortical neurons in visual V1 and MT of monkeys in strong contrast with a small $c_{vo} (= 0.05 \sim 0.1)$ in motor neurons [27]. In order to explain the large c_{vo} , several hypotheses have been proposed; a balance between excitatory and inhibitory inputs [28], the high physiological gain in the $f_o - I_i$ plot [29], correlation fluctuations in recurrent networks [30], and the active dendrite conductance [31]. By using the IF model, Feng and Brown [32] have shown that there are three kinds of behaviors of c_{vo} depending on the distribution of input ISIs: (a) c_{vo} tends to decrease for the Gaussian, uniform or truncated distribution of ISIs, (b) c_{vo} remains constant for the exponentially distributed ISIs, and (c) c_{vo} diverges to infinity when ISIs follow the Pareto distribution which has a slow-decreasing tail of $T^{-\alpha}$ ($\alpha > 0$) at large T . Case (a) was previously discussed by Marsalek, Koch, and Maunsell [33].

Figure 19 shows the dependence of c_{vo} on c_{vi} for various types of our input ISIs having been reported in previous sections. Inverted triangles denote the results for the constant ISIs (Sec. III A 2), open marks the results for input ISIs with sinusoidal modulation (Sec. III B), and filled circles, tri-

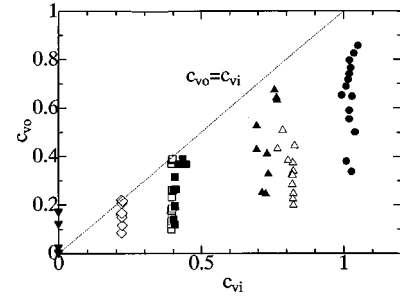


FIG. 19. c_{vo} against c_{vi} for inputs with time-independent ISI (inverted triangles, $c_{vi} = 0$), with sinusoidal modulation (open diamonds, squares, and triangles for $c_{vi} = 0.22, 0.40$, and 0.82 , respectively), and with random gamma distribution (closed squares, triangles, and circles for $c_{vi} = 0.40, 0.75$, and 1.03 , respectively). The dotted curve expressing $c_{vo} = c_{vi}$ is plotted as a guide for the eye.

angles, and squares results of the stochastic modulation (Sec. V). Our calculations show the following. (i) The constant ISI with a vanishing c_{vi} yields the finite $c_{vo} (< 0.2)$, i.e., $c_{vo} \geq c_{vi}$, (ii) the finite-width distribution of ISIs with the sinusoidal modulation leads to $c_{vo} \leq c_{vi}$, and (iii) the exponential, gamma distribution of input ISIs yield the result which is ostensibly similar to that in the item (ii). Although the item (ii) is in agreement with the result for the abovementioned case (a), the items (i) and (iii) disagree with the results of the cases of (a) and (b), respectively, discussed in Refs. [32] and [33] for IF neurons. This difference is expected to arise from the fact that the response of the type-II HH neuron with the refractory period is different from that of the type-I IF neuron without it. This is consistent with the recent calculations of Brown, Feng, and Feerick [34] for the variability of the HH and IF neurons.

Finally we want to discuss the transient response of the HH neuron to the cluster of spike-train inputs. Figures 20(a), 20(b), and 20(c) show the results for $T_{in} = 5, 10$, and 20 msec, respectively. In Fig. 20(c), for example, the upper (lower) panel of C1, C2, C3, and C4 express the time courses of input (output) spike trains for inputs of two, three, four and five impulses, respectively, with $T_{in} = 20$ msec. In this case the ISI of output pulses is the same as that of input

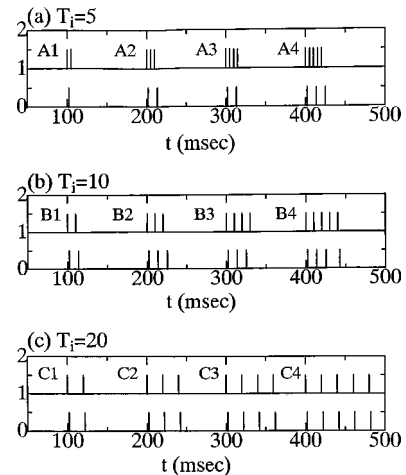


FIG. 20. Time courses of spike-train inputs and outputs; input ISIs are (a) $T_i = 5$, (b) 10 , and (c) 20 msec, and upper (lower) panel of each figure shows inputs (outputs).

pulses, $T_{om}=T_{in}$, because the HH neuron behaves as a linear transmitter for inputs with ISI of $T_{in}\geq 10$ msec. On the contrary, its behaviors of output ISI data for inputs with $T_{in}=5$ and 10 msec are much complicated. Figure 20(a) shows that output ISIs for $T_{in}=5$ msec are 11.39 and 11.87 msec, which should be compared with $T_{om}=10.94$ and 14.06 msec for the sequence of the spike trains with constant ISI of 5 msec discussed in Sec. III A 2. For the case of $T_{in}=10$ msec shown in Fig. 20(b), we get $T_{om}=11.44$, 11.80, and 17.11 msec whereas the sequence of the constant ISI of 10 msec leads to $T_{om}=11.25$, 12.36, and 16.39 msec (Fig. 5). It is noted that both inputs with three (A2) and four impulses (A3) yield the same output of two impulses. Similarly, inputs with three (B2) and four impulses (B3) lead to outputs with three impulses. We should note in all the cases shown

in Figs. 20(a)–20(c) that the first output pulse is rather quickly emitted with a delay of 2.1 msec after the first input pulse of clusters is applied to the HH neuron. This fast transient response may be relevant to a quick passage of information reported by Thorpe, Eize, and Marlot [5] and by Rolls and Tovee [6].

Note added. Recently we noticed the calculation of the variability of the HH and IF neurons in Ref. [34], whose result is consistent with ours.

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- [1] F. Rieke, D. Warland, R. Steveninck, and W. Bialek, *Exploring the Neural Code* (MIT Press, England, 1996).
 - [2] T. J. Sejnowski, *Nature (London)* **376**, 21 (1995).
 - [3] J. J. Hopfield, *Nature (London)* **376**, 33 (1995).
 - [4] D. Ferster and N. Spruston, *Science* **270**, 756 (1995).
 - [5] S. Thorpe, D. Fize, and C. Marlot, *Nature (London)* **381**, 520 (1996).
 - [6] E. T. Rolls and M. J. Tovee, *Proc. R. Soc. London, Ser. B* **257**, 9 (1994).
 - [7] W. Maass, *Neural Comput.* **9**, 279 (1997); related references are therein.
 - [8] For a review on neuron models, see W. Gerstner, *Phys. Rev. E* **51**, 738 (1995).
 - [9] A. L. Hodgkin and A. F. Huxley, *J. Physiol. (London)* **117**, 500 (1952).
 - [10] B. S. Gutkin and G. B. Ermentrout, *Neural Comput.* **10**, 1047 (1998).
 - [11] I. Nemoto, S. Miyazaki, M. Saito, and T. Utsunomiya, *Biophys. J.* **15**, 469 (1976).
 - [12] A. V. Holden, *Biol. Cybern.* **21**, 1 (1976).
 - [13] J. F. Fohlmeister, W. J. Adelman, and R. E. Poppele, *Biophys. J.* **30**, 79 (1980).
 - [14] G. Matsumoto, K. Kim, T. Ueda, and J. Shimada, *J. Phys. Soc. Jpn.* **49**, 906 (1980).
 - [15] R. Guttman, L. Feldman, and E. Jakobsson, *J. Membr. Biol.* **56**, 9 (1980).
 - [16] K. Aihara, G. Matsumoto, and Y. Ikegaya, *J. Theor. Biol.* **109**, 249 (1984).
 - [17] G. Matsumoto, K. Aihara, M. Ichikawa, and A. Tasaki, *J. Theor. Neurobiol.* **3**, 1 (1984).
 - [18] H. Hayashi, S. Ishizuka, and K. Hirakawa, *J. Phys. Soc. Jpn.* **54**, 2337 (1985).
 - [19] C. Koch and Ö. Bernander, *The Handbook of Brain Theory and Neural Networks*, edited by M. A. Arbib (MIT Press, England, 1995), pp. 129–134.
 - [20] M. Park and S. Kim, *J. Korean Phys. Soc.* **29**, 9 (1996).
 - [21] O. E. Rössler, *Phys. Lett.* **57A**, 397 (1976).
 - [22] E. Lorentz, *J. Atmos. Sci.* **20**, 131 (1963).
 - [23] J. Theiler, S. Eubank, A. Longtin, B. Galdrikian, and J. D. Farmer, *Physica D* **58**, 77 (1992).
 - [24] T. Sauer, *Phys. Rev. Lett.* **72**, 3811 (1994).
 - [25] D. M. Racicot and A. Longtin, *Physica D* **104**, 184 (1997).
 - [26] W. R. Softky and C. Koch, *Neural Comput.* **4**, 643 (1992).
 - [27] W. Calvin and C. Stevens, *J. Neurophysiol.* **31**, 574 (1968).
 - [28] M. Shadlen and W. T. Newsome, *Curr. Opin. Neurobiol.* **4**, 569 (1994).
 - [29] T. W. Troyer and K. D. Miller, *Neural Comput.* **9**, 971 (1997).
 - [30] M. Usher, M. Stemmer, C. Koch, and Z. Olami, *Neural Comput.* **6**, 795 (1994).
 - [31] W. R. Softky, *Curr. Opin. Neurobiol.* **5**, 239 (1995).
 - [32] J. Feng and D. Brown, *J. Phys. A* **31**, 1239 (1998).
 - [33] P. Marsalek, C. Koch, and J. Maunsell, *Proc. Natl. Acad. Sci. USA* **94**, 735 (1997).
 - [34] D. Brown, J. Feng, and S. Feerick, *Phys. Rev. Lett.* **82**, 4731 (1999).