## **Stochastic interpretation of** *g***-subdiffusion process**

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Recently, we considered the *g*-subdiffusion equation with a fractional Caputo time derivative with respect to another function *g*, T. Kosztołowicz *et al.* [Phys. Rev. E **104**[, 014118 \(2021\)\]](https://doi.org/10.1103/PhysRevE.104.014118). This equation offers different possibilities for modeling diffusion such as a process in which a type of diffusion evolves continuously over time. However, the equation has not been derived from a stochastic model and the stochastic interpretation of *g* subdiffusion is still unknown. In this Letter, we show the stochastic foundations of this process. We derive the equation by means of a modified continuous time random walk model. An interpretation of the *g*-subdiffusion process is also discussed.

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*Introduction*. Subdiffusion occurs in media in which the movement of diffusing molecules is very difficult due to the complex internal structure of the medium. A useful tool used in normal and anomalous diffusion modeling is the continuous time random walk (CTRW) model  $[1-15]$ , and the citation list on this issue can be significantly extended. Within this model, a distribution of time between particle jumps  $\psi$  has a heavy tail for subdiffusion,  $\psi(t) \sim 1/t^{1+\alpha}$ ,  $0 < \alpha < 1$  [\[6–17\]](#page-3-0). This model provides the "ordinary" subdiffusion equation with the fractional order Riemann-Liouville or Caputo derivative [\[10–16,18–24\]](#page-3-0). Recently, a more general subdiffusion equation with the Caputo derivative with respect to another function *g* has been considered  $[25]$  (see also Ref.  $[26]$ ); we call it the *g*-subdiffusion equation which describes the *g*-subdiffusion process. As shown in Ref. [\[25\]](#page-3-0), this equation describes a process in which a type of diffusion can change over time. As we discuss later, the *g*-subdiffusion equation can be used to describe a process in which ordinary subdiffusion is additionally slowed down. Such a process may occur, among others, in the diffusion of drugs in a system consisting of packed gel beads immersed in water [\[27\]](#page-3-0) and in the diffusion of antibiotics in a bacterial biofilm [\[28\]](#page-3-0). Unfortunately, *g* subdiffusion does not yet have a stochastic interpretation. We show how to derive the *g*-subdiffusion equation by means of a modified CTRW model and we discuss the interpretation of this process.

*"Ordinary" subdiffusion equation.* The fractional subdiffusion equation with an "ordinary" Caputo derivative of the order  $\alpha \in (0, 1)$  is [\[24\]](#page-3-0)

$$
\frac{c_{\partial^{\alpha}P(x,t)}}{\partial t^{\alpha}} = D \frac{\partial^2 P(x,t)}{\partial x^2},
$$
 (1)

where the Caputo fractional derivative is defined for  $0 < \alpha <$ 1 as

$$
\frac{c_{d^{\alpha}}}{dt^{\alpha}}f(t) = \frac{1}{\Gamma(1-\alpha)} \int_0^t (t-u)^{-\alpha} f'(u) du,
$$
 (2)

 $\alpha$  is a subdiffusion parameter, and *D* is a generalized diffusion coefficient measured in the units of  $m^2/s^{\alpha}$ . To solve the equation the Laplace transform  $\mathcal L$  can be used,

$$
\mathcal{L}[f(t)](s) = \int_0^\infty e^{-st} f(t) dt.
$$
 (3)

Due to the relation

$$
\mathcal{L}\left[\frac{^C d^{\alpha}f(t)}{dt^{\alpha}}\right](s) = s^{\alpha}\mathcal{L}[f(t)](s) - s^{\alpha-1}f(0),\tag{4}
$$

where  $0 < \alpha \leq 1$ , we get

$$
s^{\alpha} \mathcal{L}[P(x,t)](s) - s^{\alpha - 1} P(x,0) = D \frac{\partial^2 \mathcal{L}[P(x,t)](s)}{\partial x^2}.
$$
 (5)

*g-subdiffusion equation.* In this Letter, functions describing *g* subdiffusion are denoted by a tilde. The *g*-subdiffusion equation reads

$$
\frac{c_{\partial_g^{\alpha}} \tilde{P}(x,t)}{\partial t^{\alpha}} = D \frac{\partial^2 \tilde{P}(x,t)}{\partial x^2},
$$
(6)

where  $0 < \alpha < 1$ , the Caputo derivative with respect to another function *g* is defined as [\[29\]](#page-3-0)

$$
\frac{C_{d_g^{\alpha}}f(t)}{dt^{\alpha}} = \frac{1}{\Gamma(1-\alpha)} \int_0^t [g(t) - g(u)]^{-\alpha} f'(u) du, \quad (7)
$$

the function *g* fulfills the conditions  $g(0) = 0$ ,  $g(\infty) = \infty$ , and  $g'(t) > 0$  for  $t > 0$ , and its values are given in a time unit. When  $g(t) = t$ , the *g*-Caputo fractional derivative takes a form of the ordinary Caputo derivative. To solve Eq. (6) the *g*-Laplace transform can be used, and this transform is defined

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<span id="page-1-0"></span>as [\[30\]](#page-3-0)

$$
\mathcal{L}_g[\tilde{f}(t)](s) = \int_0^\infty e^{-sg(t)} \tilde{f}(t)g'(t)dt.
$$
 (8)

Due to the property [\[30\]](#page-3-0)

$$
\mathcal{L}_g \left[ \frac{^C d_g^{\alpha}}{dt^{\alpha}} \tilde{f}(t) \right] (s) = s^{\alpha} \mathcal{L}_g [\tilde{f}(t)](s) - s^{\alpha - 1} \tilde{f}(0), \qquad (9)
$$

the procedure of solving Eq.  $(6)$  is similar to the procedure of solving an ordinary subdiffusion equation by means of the ordinary Laplace transform method. In terms of the *g*-Laplace transform the *g*-subdiffusion equation is

$$
s^{\alpha} \mathcal{L}_g[\tilde{P}(x,t)](s) - s^{\alpha - 1} \tilde{P}(x,0) = D \frac{\partial^2 \mathcal{L}_g[\tilde{P}(x,t)](s)}{\partial x^2}.
$$
 (10)

Using the *g*-Laplace transform to Eq. [\(6\)](#page-0-0) yields Eq. (10) in the same form as Eq.  $(5)$ .

*Model of a particle random walk.* To derive the subdiffusion equation we use a simple model of a particle random walk along a one-dimensional homogeneous lattice. Usually, in the CTRW model both a particle jump length and waiting time for a particle jump are random variables. In our considerations, we assume that the jump length distribution  $\lambda$  has the form  $\lambda(x) = \frac{1}{2} [\delta(x - \epsilon) + \delta(x + \epsilon)]$ , where  $\delta$  is the delta Dirac function. Only the choice of a particle jump direction is random, where its length  $\epsilon$  is a parameter. We start with the particle random walk model in which the particle positions and time are discrete. Next, we move to continuous variables. A random walk with discrete time *n* is described by the equation  $P_{n+1}(m) = \frac{1}{2}P_n(m+1) + \frac{1}{2}P_n(m-1)$ , where  $P_n(m)$ is a probability that a diffusing particle is at the position *m* after the *n*th step. Let the initial particle position be  $m = 0$ . Moving from discrete *m* to continuous *x* spatial variable we assume  $x = m\epsilon$  and  $P_n(x) = P_n(m)/\epsilon$ , where  $\epsilon$  is a distance between discrete sites. The above equations and the relation  $[P_n(x+\epsilon)+P_n(x-\epsilon)-2P_n(x)]/\epsilon^2=\frac{\partial^2 P_n(x)}{\partial x^2}, \epsilon \to 0,$ provide the following equation in the limit of small  $\epsilon$ ,

$$
P_{n+1}(x) - P_n(x) = \epsilon^2 \frac{\partial^2 P_n(x)}{\partial x^2}.
$$
 (11)

To move from discrete to continuous time we use the formula  $[1]$ 

$$
P(x,t) = \sum_{n=0}^{\infty} Q_n(t) P_n(x),
$$
\n(12)

where  $Q_n(t)$  is the probability that a diffusing particle takes *n* steps in the time interval  $(0, t)$ . The function  $Q_n$  is determined differently for ordinary subdiffusion and *g* subdiffusion. In the following, we find the rule for determining the functions  $Q_n$ and the explicit form of the functions  $\psi$  for both processes. These functions, together with Eqs.  $(11)$  and  $(12)$ , provide ordinary subdiffusion and *g*-subdiffusion equations.

*The case of ordinary subdiffusion.* In this case the function  $Q_n$  is a convolution of *n* distributions  $\psi$  of a waiting time for a particle to jump and a function *U* which is the probability that a particle does not change its position after the *n*th step,

$$
Q_n(t) = \underbrace{(\psi * \psi * \cdots * \psi}_{n \text{ times}} * U)(t), \tag{13}
$$

where the convolution is defined as

$$
(f * h)(t) = \int_0^t f(u)h(t-u)du.
$$
 (14)

The ordinary Laplace transform has the following property that makes the transform useful in determining the function *Qn*,

$$
\mathcal{L}[(f * h)(t)](s) = \mathcal{L}[f(t)](s)\mathcal{L}[h(t)](s).
$$
 (15)

From Eqs.  $(12)$ ,  $(13)$ , and  $(15)$  we have

$$
\mathcal{L}[P(x,t)](s) = \mathcal{L}[U(t)](s) \sum_{n=0}^{\infty} \mathcal{L}^n[\psi(t)](s)P_n(x). \quad (16)
$$

Combining Eqs.  $(11)$ ,  $(12)$ , and  $(16)$  we get

$$
\frac{2[1 - \mathcal{L}[\psi(t)](s)]}{\epsilon^2 \mathcal{L}[\psi(t)](s)} \mathcal{L}[P(x, t)](s) - \frac{2\mathcal{L}[U(t)](s)}{\epsilon^2 \mathcal{L}[\psi(t)](s)} P(x, 0)
$$

$$
= \frac{\partial^2 \mathcal{L}[P(x, t)](s)}{\partial x^2}.
$$
(17)

Comparing Eq.  $(17)$  with Eq.  $(5)$  we conclude that they are identical only if

$$
\frac{1-\mathcal{L}[\psi(t)](s)}{\mathcal{L}[\psi(t)](s)} = \frac{\epsilon^2 s^{\alpha}}{2D}, \quad \frac{\mathcal{L}[U(t)](s)}{\mathcal{L}[\psi(t)](s)} = \frac{\epsilon^2 s^{\alpha-1}}{2D}.
$$

The solutions to the above equations are

$$
\mathcal{L}[\psi(t)](s) = \frac{1}{1 + \frac{\epsilon^2 s^{\alpha}}{2D}},\tag{18}
$$

and

$$
\mathcal{L}[U(t)](s) = \frac{\epsilon^2 s^{\alpha - 1}}{2D\left(1 + \frac{\epsilon^2 s^{\alpha}}{2D}\right)} = \frac{1 - \mathcal{L}[\psi(t)](s)}{s}.
$$
 (19)

Due to the relations

$$
\mathcal{L}[1](s) = \frac{1}{s}, \quad \mathcal{L}\left[\int_0^t f(u)du\right](s) = \frac{\mathcal{L}[f(t)](s)}{s}, \quad (20)
$$

we get

$$
U(t) = 1 - \int_0^t \psi(u) du.
$$
 (21)

In order to find the function  $\psi$  we use the relation [\[31\]](#page-3-0)

$$
\mathcal{L}^{-1}[s^{\nu}e^{-as^{\beta}}](t) = \frac{1}{t^{1+\nu}}\sum_{k=0}^{\infty}\frac{1}{k!\Gamma(-\nu-\beta k)}\left(-\frac{a}{t^{\beta}}\right)^{k}
$$

$$
\equiv f_{\nu,\beta}(t:a),\tag{22}
$$

where  $a, \beta > 0$ , and  $\Gamma$  is the Euler's gamma function. The function  $f_{\nu,\beta}$  is the Wright function and the special case of Fox's *H* function. To find the inverse Laplace transform of Eq. (18) first we calculate the inverse Laplace transform of the function  $e^{-as^{\beta}}/(1 + \tau s^{\alpha})$ , where  $\tau = \epsilon^2/2D$ and  $a, \beta > 0$ , using the formula  $1/(1 + u) = \sum_{n=0}^{\infty} u^n$  when  $|u|$  < 1. We get

$$
\mathcal{L}\left[\frac{e^{-as^{\beta}}}{1+\tau s^{\alpha}}\right](s) = \begin{cases} \frac{1}{\tau} \sum_{n=0}^{\infty} \left(-\frac{1}{\tau}\right)^{n} s^{-(n+1)\alpha} e^{-as^{\beta}}, & s > \frac{1}{\tau^{1/\alpha}},\\ \sum_{n=0}^{\infty} (-\tau)^{n} s^{n\alpha} e^{-as^{\beta}}, & s < \frac{1}{\tau^{1/\alpha}}. \end{cases}
$$
\n(23)

<span id="page-2-0"></span>Next, we take the limit of  $a \to 0$ . From Eqs. [\(22\)](#page-1-0), [\(23\)](#page-1-0), and the relations  $f_{\nu,\beta}(t;0) = 1/\Gamma(-\nu)t^{1+\nu}$ ,  $1/\Gamma(0) = 0$ , we get

$$
\psi(t) = \begin{cases} \frac{1}{\tau} \sum_{n=0}^{\infty} \left( -\frac{1}{\tau} \right)^n \frac{t^{(n+1)\alpha - 1}}{\Gamma((n+1)\alpha)}, & t < \tau^{1/\alpha}, \\ \sum_{n=0}^{\infty} \left( -\tau \right)^{n+1} \frac{t^{-(n+1)\alpha - 1}}{\Gamma(-(n+1)\alpha)}, & t > \tau^{1/\alpha}. \end{cases}
$$
(24)

We have  $\psi(t) \approx \alpha \tau / \Gamma(1-\alpha)t^{1+\alpha}$  in the limit of  $t \to$  $\infty$ . The function  $\psi$  was already derived using the relation  $\mathcal{L}^{-1}[1/(1 + \tau s^{\alpha})] = t^{\alpha-1}E_{\alpha,\alpha}(-t^{\alpha}/\tau)$ , where  $E_{\alpha,\alpha}(z) = \sum_{\alpha}^{\infty} \tau^n/\Gamma(\alpha(n+1))$  is the two-parameter Mittag-Leffler  $\sum_{n=0}^{\infty} z^n / \Gamma(\alpha(n+1))$  is the two-parameter Mittag-Leffler function (see, for example, Ref. [\[32\]](#page-3-0)). Then, the function  $\psi$ corresponds to Eq. (24) but for the case of  $t < \tau^{1/\alpha}$  only.

*The case of g subdiffusion.* To get Eq. [\(10\)](#page-1-0) we use the *g*-Laplace transform. This transform has the following property [\[30\]](#page-3-0),

$$
\mathcal{L}_g[(f *_{g} h)(t)](s) = \mathcal{L}_g[f(t)](s)\mathcal{L}_g[h(t)](s), \qquad (25)
$$

where the *g* convolution is defined as

$$
(f *_{g} h)(t) = \int_{0}^{t} f(u)h[g^{-1}(g(t) - g(u))]g'(u)du.
$$
 (26)

We involve the *g* convolution in the CTRW model. Then, the procedure for deriving the *g*-subdiffusion equation using the *g*-Laplace transform is analogous to the procedure for deriving the ordinary subdiffusion equation using the ordinary Laplace transform. Assuming

$$
\tilde{P}(x,t) = \sum_{n=0}^{\infty} \tilde{Q}_n(t) P_n(x)
$$
\n(27)

and

$$
\tilde{Q}_n(t) = (\underbrace{\tilde{\psi} *_{g} \tilde{\psi} *_{g} \cdots *_{g} \tilde{\psi} *_{g} \tilde{U}}_{n \text{ times}} *_{g} \tilde{U})(t),
$$
\n(28)

from Eqs.  $(25)$ ,  $(27)$ , and  $(28)$  we obtain

$$
\mathcal{L}_g[\tilde{P}(x,t)](s) = \sum_{n=0}^{\infty} \mathcal{L}_g[\tilde{U}(t)](s)\mathcal{L}_g^n[\tilde{\psi}(t)](s)P_n(x). \quad (29)
$$

From Eqs.  $(11)$  and  $(29)$  we get

$$
\frac{1 - \mathcal{L}_g[\tilde{\psi}(t)](s)}{\epsilon^2 \mathcal{L}_g[\tilde{\psi}(t)](s)} \mathcal{L}_g[\tilde{P}(x, t)](s) - \frac{\mathcal{L}_g[\tilde{U}(t)](s)}{\epsilon^2 \mathcal{L}_g[\tilde{\psi}(t)](s)} \tilde{P}(x, 0)
$$

$$
= \frac{\partial^2 \mathcal{L}[\tilde{P}(x, t)](s)}{\partial x^2}.
$$
(30)

Equations  $(30)$  and  $(10)$  are identical only when

$$
\mathcal{L}_g[\tilde{\psi}(t)](s) = \frac{1}{1 + \frac{\epsilon^2 s^{\alpha}}{2D}}\tag{31}
$$

and

$$
\mathcal{L}_g[\tilde{U}(t)](s) = \frac{\epsilon^2 s^{\alpha - 1}}{2D\left(1 + \frac{\epsilon^2 s^{\alpha}}{2D}\right)}.\tag{32}
$$

Comparing Eqs.  $(31)$  and  $(32)$  with Eqs.  $(18)$  and  $(19)$ , respectively, we get

$$
\mathcal{L}_g[\tilde{\psi}(t)](s) = \mathcal{L}[\psi(t)](s),\tag{33}
$$

$$
\mathcal{L}_g[\tilde{U}(t)](s) = \mathcal{L}[U(t)](s).
$$
 (34)

From the relation

$$
\mathcal{L}_g[\tilde{f}(t)](s) = \mathcal{L}[\tilde{f}(g^{-1}(t))](s),\tag{35}
$$

we get the following rule [\[25\]](#page-3-0),

$$
\mathcal{L}_g[\tilde{f}(t)](s) = \mathcal{L}[f(t)](s) \Leftrightarrow \tilde{f}(t) = f(g(t)). \tag{36}
$$

Due to Eq.  $(36)$ , from Eqs.  $(33)$  and  $(34)$  we obtain

$$
\tilde{\psi}(t) = \psi(g(t)),\tag{37}
$$

and

$$
\tilde{U}(t) = U(g(t)).\tag{38}
$$

Equations  $(24)$  and  $(37)$  provide

$$
\tilde{\psi}(t) = \begin{cases}\n\frac{1}{\tau} \sum_{n=0}^{\infty} \left( -\frac{1}{\tau} \right)^n \frac{g^{(n+1)\alpha - 1}(t)}{\Gamma((n+1)\alpha)}, & t < g^{-1}(\tau^{1/\alpha}), \\
\sum_{n=0}^{\infty} \left( -\tau \right)^{n+1} \frac{g^{-(n+1)\alpha - 1}(t)}{\Gamma(-(n+1)\alpha)}, & t > g^{-1}(\tau^{1/\alpha}).\n\end{cases} \tag{39}
$$

We get  $\tilde{\psi}(t) \approx \alpha \tau / \Gamma(1 - \alpha) g^{1 + \alpha}(t)$  when  $t \to \infty$ .

We link the *g* convolution with the ordinary convolution. Let  $\tilde{f}(t) = f(g(t))$  and  $\tilde{h}(t) = h(g(t))$ . After simple calculation we get

$$
(\tilde{f} *_{g} \tilde{h})(t) = (f * h)(g(t)).
$$
\n(40)

From Eqs. (27), (28), and (40) we have

$$
\tilde{P}(x,t) = \sum_{n=0}^{\infty} Q_n(g(t))P_n(x).
$$
\n(41)

Comparing Eqs.  $(41)$  and  $(12)$  we obtain

$$
\tilde{P}(x,t) = P(x,g(t)).\tag{42}
$$

*Interpretation.* The *g*-subdiffusion process is associated to ordinary subdiffusion controlled by the same parameter  $\alpha$ . The waiting time for a particle jump in the *g*-subdiffusion process is controlled by the functions  $\psi$  and *g*. A particle jump that would occur with some probability after time *t* in an ordinary subdiffusion process will occur with the same probability after time  $\tilde{t} = g^{-1}(t)$  in the *g*-subdiffusion process. If  $g(t) < t$ , we have  $t < \tilde{t}$ , and subdiffusion is then slowed down. When  $g(t) > t$ , subdiffusion is accelerated.

An example of *g* subdiffusion is the diffusion of molecules in a medium consisting of a matrix in which there are narrow channels. If the channels have a complicated geometric structure and diffusing molecules do not interact with the matrix, then ordinary subdiffusion controlled by the parameter  $\alpha$  occurs. If the matrix provides the diffusing molecules with additional energy, subdiffusion can be accelerated. When temporary penetration of a molecule into the matrix is possible, then the molecule "disappears" from the channels and may diffuse further upon returning to a channel. In this case, ordinary subdiffusion is slowed down. Such a process occurs in a vessel filled with alginate beads immersed in water in which a colistin antibiotic diffuses [\[27\]](#page-3-0). Other examples of the possible application of the *g*-subdiffusion equation is the diffusion of drugs [\[33–36\]](#page-3-0) or fertilizers [\[37](#page-3-0)[–39\]](#page-4-0) in systems consisting of beads immersed in water. We also suppose that the *g*subdiffusion model can be used to describe the diffusion of antibiotics in a biofilm. Biofilms usually have a gel structure. When the antibiotic does not interact with bacteria, ordinary antibiotic subdiffusion in the biofilm is expected. However,

<span id="page-3-0"></span>bacteria in the biofilm have different defense mechanisms against the action of the antibiotic. These mechanisms may hinder or even facilitate antibiotic subdiffusion (see Ref. [28] and the references cited therein). Thus, the application of the *g*-subdiffusion equation to describe this process may be effective.

*Final remarks.* We have shown that the *g*-subdiffusion equation can be derived by means of the modified CTRW model (we call it the *g*-CTRW model). In the *g*-CTRW model we use *g* convolution and the *g*-Laplace transform instead of "ordinary" convolution and the "ordinary" Laplace transform, respectively, which are used in the "ordinary" CTRW model.

We note that the condition  $\mathcal{L}_{g}[\psi(t)](0) = 1$  does not guarantee that the function  $\tilde{\psi}$  is normalized. Therefore,  $\tilde{\psi}$  is not a probability distribution. Thus, it seems that the *g*-CTRW model is merely a mathematical procedure. However, this model can be interpreted as an ordinary CTRW model in

which the timescale is controlled by the function  $g(t)$  [see Eqs. [\(37\)](#page-2-0)–[\(42\)](#page-2-0)]. The key issue for the *g*-subdiffusion process is determining the parameter  $\alpha$  and the function *g*. An example of their determination from empirical data is shown in Ref. [27].

In practice, the transformations made in deriving the *g*subdiffusion equation within the *g*-CTRW model are the same as in deriving the ordinary subdiffusion equation using ordinary CTRW. Within the ordinary CTRW, subdiffusionreaction equations [\[40\]](#page-4-0) as well as the Green's functions and membrane boundary conditions for a system in which a thin membrane separates different subdiffusive media [\[41\]](#page-4-0) have been derived. Within the *g*-CTRW model the same procedures can also be used to derive *g*-subdiffusion-reaction equations, Green's functions, and boundary conditions at the membrane for the processes described by *g*-subdiffusion equations.

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