Near-field studies of anisotropic variations and temperature-induced structural changes in a supported single lipid bilayer

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Temperature-controlled polarization modulation near-field scanning optical microscopy measurements of a single supported $L_{\beta'}$ 1,2-dipalmitoyl-sn-glycero-3-phosphocholine (DPPC) lipid bilayer are presented. The effective retardance $(S = \frac{2\pi(n_e - n_o)t}{\lambda})$, where t is the thickness of the bilayer and λ is the wavelength of light used) and the direction of the projection of the acyl chains (θ) were measured simultaneously. We demonstrate how one is able to align the system over the sample and measure a relative retardance ΔS , a crucial step in performing temperature-controlled experiments. Maps of ΔS and θ , with a lateral resolution on the order of ~ 100 nm are presented, highlighting variations deriving from changes in the average molecular orientation across a lipid membrane at room temperature. A discussion of how this information can be used to map the average three-dimensional orientation of the molecules is presented. From ΔS and the known thickness of the membrane t the birefringence $(n_e - n_a)$ of the bilayer was determined. Temperature-controlled measurements yielded a change of $\Delta S \sim (3.8 \pm 0.3)$ mrad at the main transition temperature $(T_m \sim 41^{\circ}\text{C})$ of a single planar bilayer of DPPC, where the membrane transitioned between the gel $L_{\beta'}$ to liquid disorder L_{α} state. The result agrees well with previous values of $(n_e - n_o)$ in the $L_{\beta'}$ phase and translates to an assumed average acyl chain orientation relative to the membrane normal ($\langle \phi \rangle \sim 32^\circ$) when $T < T_m$ and 0° when $T > T_m$. Evidence of super heating and cooling are presented. A discussion on how the observed behavior as T_m is approached, could relate to the existence of varying microconfigurations within the lipid bilyer are presented. This conversation includes ideas from a Landau-Ginzburg picture of first-order phase transitions in nematic-to-isotropic systems.

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I. INTRODUCTION

Charting the complex interface of biological membranes is arguably the most essential piece in determining how localized interactions contribute to overall cellular function. These membranes contain an elaborate mesh of membrane proteins, various lipids, and an assortment of domains. Studying the regional lipid orientation within membranes could provide us with a better insight on the interactions between neighboring molecules. Instead of approaching the complexities of a true cellular membrane, model membranes systems are often used. These model membrane structures have been characterized using techniques ranging from nuclear magnetic resonance (NMR) to various x-ray methods [1-5]. These routines accurately predict structural properties of lipid membrane multilayers and have given us a better understanding of the physical behavior of these systems. Techniques such as NMR and x-ray scattering are not commonly used on low curvature-single bilayer systems, which are naturally found in biological cellular membranes. In general these methodologies are limited in obtaining localized lateral information of planar membrane systems.

Many groups have chosen methods that mainly focus on exploiting the anisotropic nature of lipids to obtain structural information of the lipid molecules in the membrane [3,6-9]. Techniques ranging from ellipsometry [10] to surface plasmonic resonance [11] exploit the birefringent properties of lipid bilayers to study membrane structure. More specifically, various studies have used the anisotropic properties of 1,2-dipalmitoyl-sn-glycero-3-phosphocholine (DPPC) bilayers in the $L_{\beta'}$ gel state to measure the effective retardance of the membrane system [9,12,13]. Under these conditions the lipid molecules are assumed to possess an average constant molecular tilt, $\phi \sim 32^{\circ}$ [14], across the structure. Knowing the perpendicular component of the refractive index n_{\perp} of the acyl chains, the optical orientation θ and parallel refractive index n_{\parallel} of the acyl chains can be determined. From this information one is able to resolve changes in the properties of the membrane. All mentioned techniques were utilized in studying both bulk and planar lipid membrane systems. One common drawback is that they are all limited in the lateral information they can obtain. To address this issue Lee *et al.* [12] were able to explore these structural properties by measuring the effective retardance, using a near-field scanning optical microscope (NSOM). Using NSOM one is able to obtain optical information on the order of the size of the aperature of the NSOM probe. This gave Lee et al. a lateral resolution on the order of ~ 100 nm across the planar membrane system. Though they were able to obtain a high lateral sensitivity using NSOM, the measurement of the retardance was precision limited, leaving room for improvement on the detectability of the acyl chain tilt variations across planar membrane systems.

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In an attempt to advance this work, Johnson *et al.* [15] implemented a polarization modulation (PM) technique to study topological defects across the membrane, which only slightly improved on the previous measurements conducted by Lee *et al.* [12].

In studying lipid systems it is also common to investigate their thermodynamic properties to better understand the localized interactions that take place between molecules. Temperature-controlled NMR and x-ray experiments [1,5,16–18], in addition to differential scanning calorimetry [5,19,20] have been used to study the first-order phase transitions in lipid systems. As an example, one can study the main transition from the gel $L_{\beta'}$ to liquid disordered L_{α} state in phosphocholine lipid membranes with saturated acly chains. For systems like DPPC bilayers the average orientation with respect to the normal direction of the membrane surface goes from having some characteristic tilt to having an average orientation along the normal direction. Detecting these structural changes could allow one to determine the phase transition conditions of the system.

In this paper, we will highlight an improved polarization modulation technique [21] that was combined with a temperature-controlled near-field scanning optical microscope (PM-NSOM). We will discuss how the system was calibrated and showcase how one is able to measure the relative change in the retardance (ΔS) versus an absolute retardance to improve the sensitivity of the measurement. We will also highlight how this was imperative in performing temperature-based polarization measurements on supported membrane samples. We will describe how one is able to not only obtain the average orientation of the acyl chains with respect to the membrane's normal, but also the direction of the acyl chain projection in the plane perpendicular to the membrane's normal. These attributes will be displayed using images that highlight the edge effects near defects in a planar membrane. The retardance in a supported DPPC bilayer was investigated as a function of temperature. The improvement in the apparatus yielded an enhanced precision in the retardance of a single DPPC bilayer, resulting in a more accurate difference between n_{\parallel} and n_{\parallel} over a lateral size of \sim 100 nm. Furthermore, the gel-liquid crystalline phase transition of DPPC has been investigated with the same spatial resolution. These systems were also studied as they were superheated and cooled. The results from these measurements will be discussed. We expect that the technique presented here could help with future investigations in determining the sizedependent transition temperature in mixtures of in-miscible lipids in planar bilayer systems. This will provide a new tool to investigate the intermolecular interactions between different lipids, which may address many of the previous described limitations found in other techniques [1-3,17,18].

II. EXPERIMENTAL DETAILS

A. Sample preparation

Hydrophilic glass substrates were prepared by sonicating Fisher brand glass cover slips in detergent and deionized (DI) water separately for \sim 15–20 min each. This was followed with a wet-chemical oxidation process using a piranha



FIG. 1. AFM image of supported DPPC bilayers near an edge. (a) 2.6 μ m × 2.6 μ m topographical contrast image. The low height regions represent the underlying glass slide. (b) Plot of the height data taken from a line cut 1 of the image in (a), showing a height difference of \approx 5.2 nm.

solution (H₂SO₄:H₂O₂ = 3:1) for \approx 5 min [22,23], to create a flat hydrophobic surface. The cover slips were then rinsed and sonicated for \sim 30 min in DI water and finally thermally dried under normal atmospheric conditions.

Supported lipid bilayers were formed on the prepared hydrophilic glass substrates by vesicle fusion [23,24]; 1.0– 0.5 mg/ml of 1,2-dipalmitoyl-sn-glycero-3-phosphocholine (DPPC) in 100 mM NaCl : 30 mM NaH₂PO₄ was sonicated at $\approx 60^{\circ}$ C until clear to create small unilamellar vesicles (SUV's); 100 μ L of solution was placed on the glass substrates and left to equilibrate at room temperature for ≈ 30 min. The samples were then baked at 60°C for 45– 60 min. After rinsing the samples with DI water, they were either rehydrated and characterized with an AFM under a fluid cell (see Fig. 1), or kept in a chamber at 100% relative humidity until imaged with the PM-NSOM system.

B. Experimental setup and supporting details

NSOM probes were created by heating and pulling stripped single-mode optical fiber with a micropipette puller (SU-P2000 Sutter instruments). All probes utilized in experiments were coated with ~ 5 nm of Cr and $\approx 150-200$ nm of Al. The tip diameters were determined to be \approx 80–100 nm (characterized using a scanning electron microscope). All experimental probes' polarization behavior was characterized using a universal polarizer and analyzing linear polarizer. Only NSOM probes with polarization extinction ratios that were at least 100:1 were considered acceptable and utilized in the system. The total PM-NSOM setup is schematically shown in Fig. 2. Monochromatic light from a (5-6 mW) helium neon laser ($\lambda = 632.8$ nm) was mechanically chopped and passed through a linear polarizer. All other optical elements were positioned with respect to this direction defined to be 0° . After the linear polarizer, light passed through a photoelastic modulator (PEM) (45°, frequency 41.9 kHz) and quarter wave plate (QWP) (0°) . The light was then coupled into a single-mode optical fiber, which was connected to a universal fiber polarizer, used to control the polarization going into the NSOM probe [21]. The NSOM tip-to-sample distance $(\sim 10 \text{ nm})$ was controlled utilizing a shear force feedback system [25,26]. The light from the NSOM probe and sample was collected with an objective lens, and sent through a QWP (0°) , an analyzer (-45°) , and finally collected by a Si PIN diode detector. The current from the diode was converted to a voltage signal by means of a transimpedance amplifier and measured by three lock-in amplifiers (LIA). The three LIAs were locked at the frequency of the mechanical chopper (proportional to the intensity of the laser, DC value), the first and second harmonics of the PEM frequency, respectively.

In the absence of a sample, it was initially assumed that the universal polarizer negated any polarizing effects from the fiber and NSOM probe. Under these circumstances, a Jones matrix formalism was applied and it was determined that the signal at the detector is proportional to $\frac{1}{2} - \frac{1}{2}\sin(A)\sin(S)\cos(2\theta) + \frac{1}{2}\cos(A)\sin(S)\sin(2\theta)$, where $A = B\cos(\omega t)$, *B* is the magnitude of the retardance, and ω is the angular frequency set by the PEM (The PEM was calibrated such that the Bessel function of the first kind, $J_0(B) = 0$). The lock-in amplifiers are used to obtain a signal normalized by the DC term at the first harmonic (I_{ω}) and the second harmonic $(I_{2\omega})$,

$$I_{\omega} = \gamma J_1(B) \sin(S) \cos(2\theta), \qquad (1)$$

$$I_{2\omega} = \gamma J_2(B) \sin(S) \sin(2\theta), \qquad (2)$$

where $J_1(B)$ and $J_2(B)$ are Bessel functions of the first kind, which appear due to the sinusoidal temporal dependence on A. Hence,

$$\theta = \frac{1}{2} \arctan\left(\frac{-I_{2\omega} J_1(B)}{I_{\omega} J_2(B)}\right),\tag{3}$$

and the retardance S is

$$S = \arcsin\left(\frac{I_{\omega}}{\gamma J_1(B)\cos(2\theta)}\right)$$
$$= \arcsin\left(\frac{-I_{2\omega}}{\gamma J_2(B)\sin(2\theta)}\right), \tag{4}$$

where γ is a the term associated with the lock-in measurement (i.e., $\gamma = \frac{\pi}{2}$ due to the DC component being a square wave for our study). During the alignment process in the absence of a





FIG. 2. Diagram of PM-NSOM setup. (a) PM-NSOM setup highlighted with components for room temperature studies (b) Diagram of the temperature-controlled chamber with water trough to maintain 100% relative humidity. (c) and (d) Photographs of the temperature-controlled chamber.

sample, both I_{ω} and $I_{2\omega}$ in Eqs. (1) and (2) are minimized, which implies that the retardances associated with the NSOM probe and fiber approach zero.

Moving the sample in and out of the optical path while aligning the NSOM system is not ideal due to the user's risk of damaging the probe and the cumbersome process of attaching a replacement. It would be advantageous to have a method where the alignment could be made over the sample of unknown retardance. To understand this effect, the sample and probe were modeled as two independent retarding elements, with retardances S and δ inserted between the two QWP in the previously described setup. Following the same Jones matrix formalism the expected intensities of the two retarding objects S and δ oriented at different angles were calculated. During the alignment process, where I_{ω} and $I_{2\omega}$ are minimized, we can assume the orientation of the NSOM probe/fiber and sample are equivalent. Using the assumption that the changes in retardances measured were relativly small in magnitude, the intensities,

and

$$J_{2\mu} = \gamma J_2(B) \sin(S + \delta) \sin(2\theta) \tag{6}$$

(5)

are obtained. From these expressions, it is seen that instead of an absolute retardance value, the result is the sum of the two retarding objects. Therefore, one is able to align the system over the sample using the universal polarizer, making $S + \delta \rightarrow 0$, and obtain a deviation in the retardance ΔS and a relative orientation θ across a given sample.

 $I_{\omega} = \gamma J_1(B) \sin(S + \delta) \cos(2\theta),$

To ensure the correctness of our calibration approach and the viability of our previous calculations, PM-NSOM measurements were conducted on cleaved stepped muscovite (mica) substrates. The mica substrate showed steps of different heights corresponding to a different number of layers of the crystal. Both far-field and near-field measurements were made of the retardance S on mica; the far-field measurements were used to make sure NSOM determinations were accurate. Both aforementioned approaches for measuring the retardance and orientation using the NSOM apparatus were performed. It was observed that on average the overall difference was $\Delta S \sim 0.3$ mrad between the two methods; see Fig. 3. Using the height topography from the NSOM measurement the birefringence of the muscovite crystal was determined to be ~ 0.0025 , which falls within accepted values [27,28]. It was noted that the images taken with the system aligned over the sample yielded more detail in ΔS than just measuring S. We suspect that this increase in sensitivity to sample variations is a consequence of the measurements being done from a minimum instead of an offset signal, highlighting an additional advantage of aligning the system over the sample.

All of the supported lipid bilayer experiments were conducted at 100% relative humidity, to ensure membrane structure contained the characteristic acyl chain tilt of $\approx 32^{\circ}$ in the $L_{\beta'}$ phase at room temperature. The measurements were taken with scan times ranging from 100 to 450 ms per point, where $I_{1\omega}$, $I_{2\omega}$, and topography data were collected using a data acquisition board and LABVIEW computer program. Trace and retrace images were collected to confirm measurement reliability.

Temperature-controlled PM-NSOM measurements were performed similarly to those conducted at room temperature, but included the following procedures. A cylindrical



FIG. 3. PM-NSOM picture of muscovite. (a) ΔS as a function of position with the system aligned over the sample. (b) θ as a function of position with the system aligned over the sample. (c) Graph of the distributions of the values of *S* and ΔS at different regions of the muscovite crystal. Histograms of *S* and ΔS values were made, where Gaussian curves were fit to the peaks of the results. (Dashed line) Measurements of the sample where the system was not aligned over the sample (*S*). (Solid gray line) Measurements of the sample where the system was aligned over the sample (ΔS). (Inset) Height as a function of position of the line shown in (a).

aluminum chamber with a narrow slit in one side for accommodating the NSOM probe holder was placed around the NSOM probe (Fig. 2) to minimize the lateral heat gradients across the sample. The chamber was thermally isolated with an insulating foam casing and the temperature was controlled using a Peltier thermoelectric cooler (TEC) to move thermal energy in and out of the chamber. The temperature of the sample was measured using a calibrated thermistor embedded into the aluminum sample holder. Thermistors were calibrated utilizing boiling points of deionized water, ethanol, isopropanol, methanol, and acetone. The sample holder rested on a Delrin stand with a stainless steel bottom to improve mechanical stability. With this design the temperature stability was within $\pm 0.07^{\circ}$ C. A water trough surrounded the sample holder, which preserved the required 100% relative humidity.

During a typical run the chamber's temperature was first heated beyond T_m to ensure the lipid membrane was well into the L_{α} state. The NSOM probe was then engaged with the sample. The chamber was cooled below T_m and heated back to the initial temperature. This was proven to be the most reliable method to counter the probe crashing events that occurred due to the thermal expansion of the Delrin separator.



FIG. 4. Pictorial representation of the lipid molecule and its indicatrix. The image highlights how the molecule orientation is described in terms of θ , optical orientation (ϕ), and perpendicular and parallel indices of refraction.

III. RESULTS

The anisotropic nature of lipids yields differences in the index of refraction [or birefringence $(n_e - n_o)$] along orthogonal directions in the plane of the membrane's surface. Because the polarizability of the lipid molecule is asymmetric, the refractive indices along the length of the acyl chains (n_{\parallel}) and perpendicular (n_{\perp}) are not equal. In this study, the principal optical axis is assumed to lie parallel to the length of the acyl chains, $\phi \sim 32^{\circ}$ with respect to the membranes' normal for DPPC; see a representation of the lipid molecule in Fig. 4. For all calculations, n_{\parallel} was assumed to be 1.4 [12]. Polarized light of wavelength λ propagating in the *z* direction, parallel to the membranes' normal, experiences a retardance between the *x* and *y* components of the electric field according to [12]

$$\Delta S = \frac{2\pi (n_e - n_o)t}{\lambda}$$

$$= \frac{2\pi t}{\lambda} \frac{1}{\sin\left(\arctan\left(\frac{n_{\parallel}^2}{n_{\perp}^2}\cot(\phi)\right) + \phi\right)}$$

$$\times \frac{n_{\perp}n_{\parallel}}{\sqrt{n_{\perp}^2\sin^2(\phi) + n_{\parallel}^2\cos^2(\phi)}} - n_{\perp}.$$
(7)

The extraordinary ray corresponds to the electric field parallel to the optical axis, where the electric field direction for the ordinary ray is perpendicular to that axis. Due to the small thickness of the membrane, the two rays were indistinguishable with the collection optics used.

Various images were collected from different areas of the supported DPPC bilayer on glass until a discontinuity in ΔS and θ were found. From the image of ΔS in Fig. 5, a measured change in ΔS of $\approx (3.9 \pm 0.4 \text{ mrad})$ was obtained, between a region with no membrane and membrane. This was done by taking a line cut of the image and averaging ΔS inside the





FIG. 5. PM-NSOM picture of DPPC supported on glass. (a) ΔS as a function of position. (Inset) Data taken from the line cut shown on the image. (b) Quiver-contour map of θ . (Note that the angle of the quivers was increased by a factor of 5 to enhance the changes in θ across the sample.)

hole and subtracting from a region away from the determined edge. θ is plotted using a contour plot along with quivers to show the relative projection of the acyl chains. The angle of the quivers were multiplied by a factor of five to enhance the changes detected across the sample. The contour plot highlights the boundaries of the areas with similar values. The hole was easily observed using the contour plot of θ . θ inside the hole is defined by the direction of the system's axis. The birefringence was determined to be $(n_e - n_o) = \frac{\Delta S\lambda}{2\pi t} \approx$ 0.073 ± 0.008 , using $\lambda = 632.8$ nm and $t = (5.2 \pm 0.4 \text{ nm})$ [29]. These results agree well with previous measurements with a significant reduction in error [12]. Furthermore an increase in ΔS to ≈ 7.5 mrad was obtained at the edge of the hole. It is expected that ϕ is greater where the membrane forms a boundary. The topography data did not show any change in height, which is expected since the hole is much smaller than the tip diameter, ≈ 500 nm (data is not shown).

A series of temperature PM-NSOM experiments (Fig. 6) probed the main phase transition temperature $T_m \sim 41^{\circ}$ C of DPPC across a 512 nm \times 512 nm area. The 16 \times 16 pixel raster scanned images were taken over ≈ 3.5 min, heating at a rate of ~ 0.06 °C/min. The temperature is changing as a function of time. Therefore, each pixel represents a slightly different temperature change ~ 0.8 mK. We assume the temperature to be constant over the pixel acquisition time $(\approx 0.8 \text{ s})$ due to our sensitivity limits in temperature. The full series started at $T \approx 38^{\circ}$ and finished at $T \approx 42^{\circ}$. Figure 6 highlights the main transition ocurring over a single image in the series. In Fig. 6(a), ΔS is observed to remain constant at low T and then shows a jump of $\Delta S \approx (3.84 \pm 0.20)$ mrad at \approx 41.1°C. This change in ΔS is interpreted as the average position of the acyl chains change from their characteristic $\langle \phi \rangle$ of $\approx 32^{\circ}$ in the $L_{\beta'}$ to the $\langle \phi \rangle \to 0$ in the L_{α} state. A change of $\approx 21^{\circ}$ at T_m was observed in θ at the same position ΔS transitioned at in Fig. 6, (θ data not displayed). This change in θ corresponds to the sample in the $L_{\beta'}$ state with the optical system having one θ , and changing to a different value, characteristic of the optical system, when $T > T_m$.

Using the model previously presented and the data in Fig. 6(a) we created a three-dimensional representation of the average direction of the orientation of the acyl chains of the lipid molecules within the membrane; see Fig. 6(c). Using the values for n_{\perp} and n_{\parallel} , the average orientation ϕ of the acyl chains across the NSOM probe's aperture with respect to the membrane is below T_m , $\langle \phi \rangle$ was $\approx 32^\circ$ while when it is heated above the phase transition temperature it was in the L_{α} phase, where $\langle \phi \rangle$ is zero.

The next series of temperature-controlled experiments decreased the image acquisition time to ≈ 50 s, the rate of temperature change was $\sim 5^{\circ}C/h$ over the entire scan. This was done to explore the hysteresis effects of the first-order phase transition of the planar membrane system. Images taken were identical in size to the previous described temperaturecontrolled experiments. The average ΔS of each image was taken and plotted as a function of temperature, with the error bar representing the variation across the image at that temperature. The results for ΔS are seen in Fig. 7, where a change in ΔS of ≈ 3.5 mrad was observed across T_m . Figure 7(a) shows that $S \approx 4.7$ mrad for $T < T_m$ and ≈ 1 mrad when $T > T_m$. This translates to the acyl chains $\langle \phi \rangle$ transitioning from $\sim 32^{\circ}$ to zero, calculated using Eq. (7), as is expected to occur when the lipid bilayer goes from the $L_{\beta'}$ into the L_{α} phase. We do note that in our measurements when $T < T_M$ that bilayer should exhibit properties of the ripple phase. However, due to the ripple period being smaller than the aperture of the NSOM probe, we are unable to report on the phenomena [30,31].

IV. DISCUSSION

With the knowledge obtained from the PM-NSOM experiments at room temperature on supported DPPC in the $L_{\beta'}$ phase, physical parameters about the lipid molecules in the membrane are extracted. Using the birefringence we obtain information on the polarizability of the lipid molecules. Fol-



(c)

FIG. 6. (a) Temperature-controlled PM-NSOM 512 nm×512 nm images of DPPC supported on glass. The images were raster scanned, starting from the bottom right corner of the image, with an ≈ 0.8 -s pixel acquisition time. We assumed a homogeneous temperature over the acquisition time for each pixel. An image of the measured ΔS , showing a change in ΔS of $\approx 3.8 \pm 0.3$ mrad at the T_m . This change in ΔS indicates a change of ϕ of the acyl chains. The temperature scale on the left side highlights the initial temperature of the first pixel and the temperature where we observed a transition in ΔS . (b) Graph of the calculated ϕ as a function of position using data taken in the region of the dashed line in (a). (c) Three-dimensional representation of the average acyl chain orientation throughout the membrane. Each tube portrays the average position of many lipid molecules contained in an $\sim (100 \text{ nm})^2$ area.



FIG. 7. ΔS values from a temperature-controlled PM-NSOM measurement of DPPC supported on glass. (a) Graph of ΔS_{avg} versus temperature as the system was heated, taken from $(512 \text{ nm})^2$ images showing a change in ΔS across T_m of $\approx 4.0 \pm 0.4$ mrad. (b) Cooling data graph of ΔS_{avg} versus temperature, taken from $\sim (100 \text{ nm})^2$ images.

lowing the model of rigid cylinders used by Salamon *et al.* [9] Eq. (7) and the relationship $n_i^2 = \frac{\alpha_i \epsilon_o}{(V - \alpha_i L_i)} + \epsilon_o$ (where *V* is volume and L_i is the shape factor for a cylinder [32]) we were able to determine the transverse (α_t) and longitudinal (α_l) polarizabilites. The values for the two acyl chains were determined to be $\alpha_t = 44.2$ Å³ and $\alpha_l = 94.4$ Å³ assuming the area per lipid (*A*) and acyl chain length (*l*) to be 47.9 Å² and 17.2 Å, respectively [14]. These values are very close to the theoretically calculated polarizabilities $\alpha_t = 25.14$ Å³ and $\alpha_l = 45.8$ Å³ [9,32] of a single palmitic acid C₁₆.

The hysteresis observed under the applied heating rates are comparable to what has previously been reported [19,33]. To investigate the localized homogeneity of the sample in Fig. 7(a), the variance $(\sigma_{\Delta S}^2)$ of a 150 nm × 150 nm region was analyzed. From the results, we observed that $\langle \Delta S \rangle$ fluctuated as T_m was approached; see Fig. 7. This phenomena is further highlighted in the graph of the variance versus temperature; see Fig. 8(b). We can attempt to explain these fluctuations using two avenues of thought. One could derive from the observation of varying microconfigurations that increase in number as T_m is approached, as predicted by previous computational work on lipid phase transitions [34,35]. Unfortunately, the



FIG. 8. (a) Graphical depiction of the free energy of a system as a function of the order parameter(Γ). (b) Graph of $\sigma_{\Delta S}^2$ versus *T*, created by analyzing the heating data presented in Fig. 7(a).

time scale of our measurement compounded by the probe size does not allow us to confirm these microconfiguration fluctuations with PM-NSOM. It only allows us the opportunity to speculate from the current results. The other utilizes a Landau-Ginzburg picture of the first-order phase transition in nematic-to-isotropic systems [36]. It is expected that as the system crosses the melting temperature (T_m) and approaches the super-cooled or super-heated temperature (T^*) the shape of the free energy curve changes, as shown in Fig. 8(a), where the free energy is depicted as a function of the order parameter (Γ). In the process of heating, where T is beyond T_m , the free energy functional shape and width of the metastable minimum slightly increases, allowing for an increase in the fluctuations of Γ and consequently of any thermodynamic quantity. The deviations from the mean in Γ increase and therefore can be correlated to the subtle growth in the value of $\sigma_{\Delta S}^2$ as the system approached T^* . The increase in the variance in ΔS correlates with an oscillation in state variability from Fig. 8(a). It can be clearly seen that before the system reaches T_m , $\sigma_{\Delta S}^2$ is smaller in magnitude than when the system approaches T^* $(\sim 42^{\circ}C)$. This may suggest that this observation highlights these fluctuations in the metastable region predicted in the Landau-Ginzburg model, which will be further investigated in future work.

V. CONCLUSIONS

PM-NSOM was utilized in determining the anisotropic structural properties in supported lipid bilayers. The technique was shown to improve previous measurements on *S* by measuring ΔS and independently determining the direction of the projection of the acyl chains onto the membrane's surface. It was also shown that one can obtain accurate lateral high resolution ΔS and orientation images with the PM-NSOM system while aligning the system over the sample. With that increased sensitivity, the longitudinal and transverse polarizability were more accurately determined yielding results comparable to their theoretically calculated values. In addition, having this sensitivity proved to be imperative in conducting the temperature-controlled experiments and allowed one to measure relative values of ΔS and θ .

By adding temperature control to PM-NSOM the main phase transition from the gel state to the liquid disorder phase was observed in a planar supported bilayer with a lateral resolution ~ 100 nm. The melting temperature of a single DPPC lipid bilayer was found to be in good agreement with previously reported work. The information from ΔS and θ allowed for the creation of a three-dimensional model of the average orientation of the lipid molecules within the membrane. The system's sensitivity and control allowed for the observations of increased fluctuations as the metastable region of the phase diagram of the lipid membrane was probed. Future work could extend into membrane systems containing lipid mixtures or even protein-lipid complexes, where the properties of domains with different phases or orientations may be explored. With temperature control, the lateral dynamics of phase separations or even changes in the orientation of the lipid bilayer through regions of interest could be observed. Overall it was shown how PM-NSOM can be utilized as a highly sensitive and noninvasive technique to study single lipid bilayer systems and achieve structural information beyond the ability of conventional optical techniques.

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